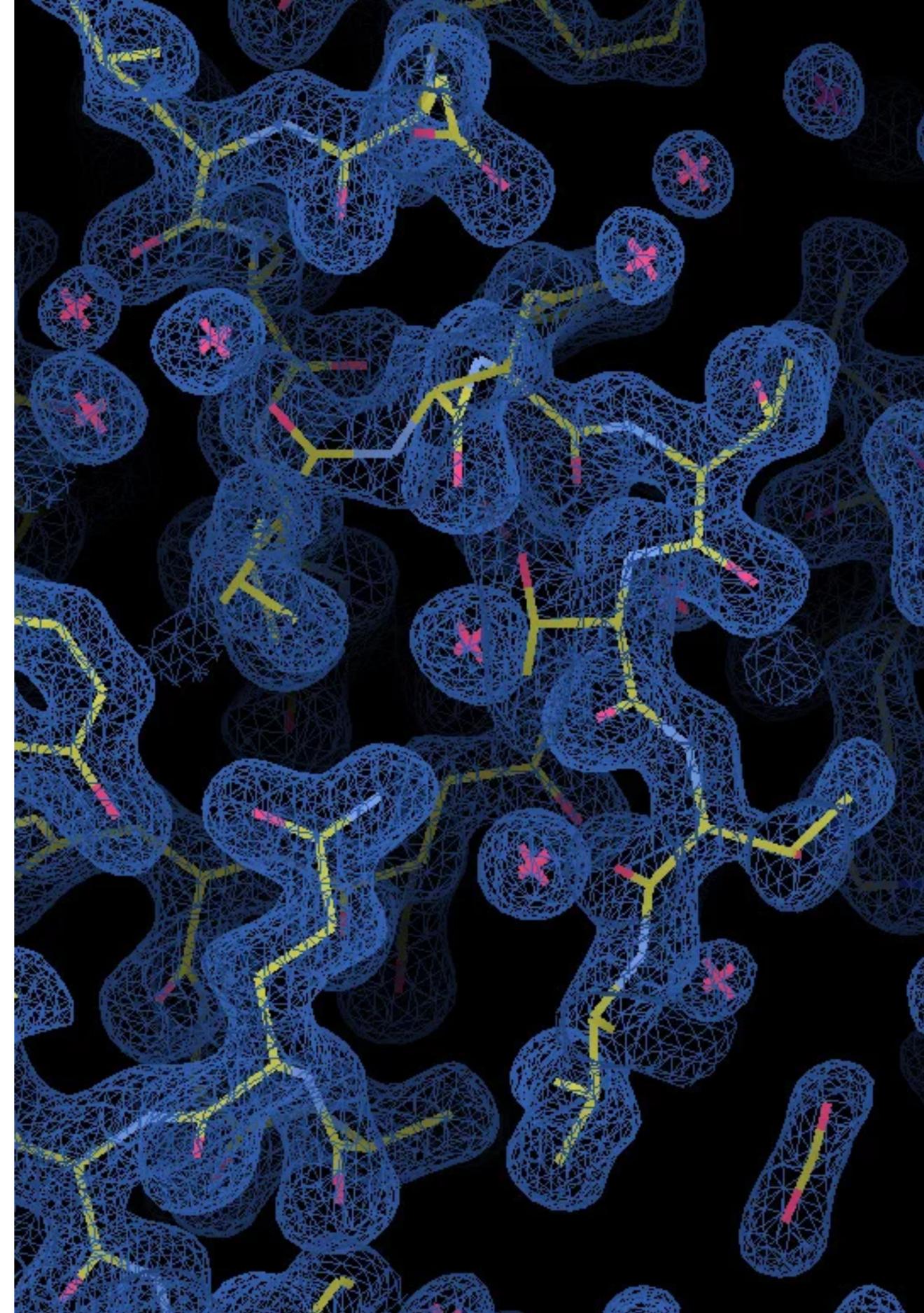


Protein Structure Determination with Cryo-EM

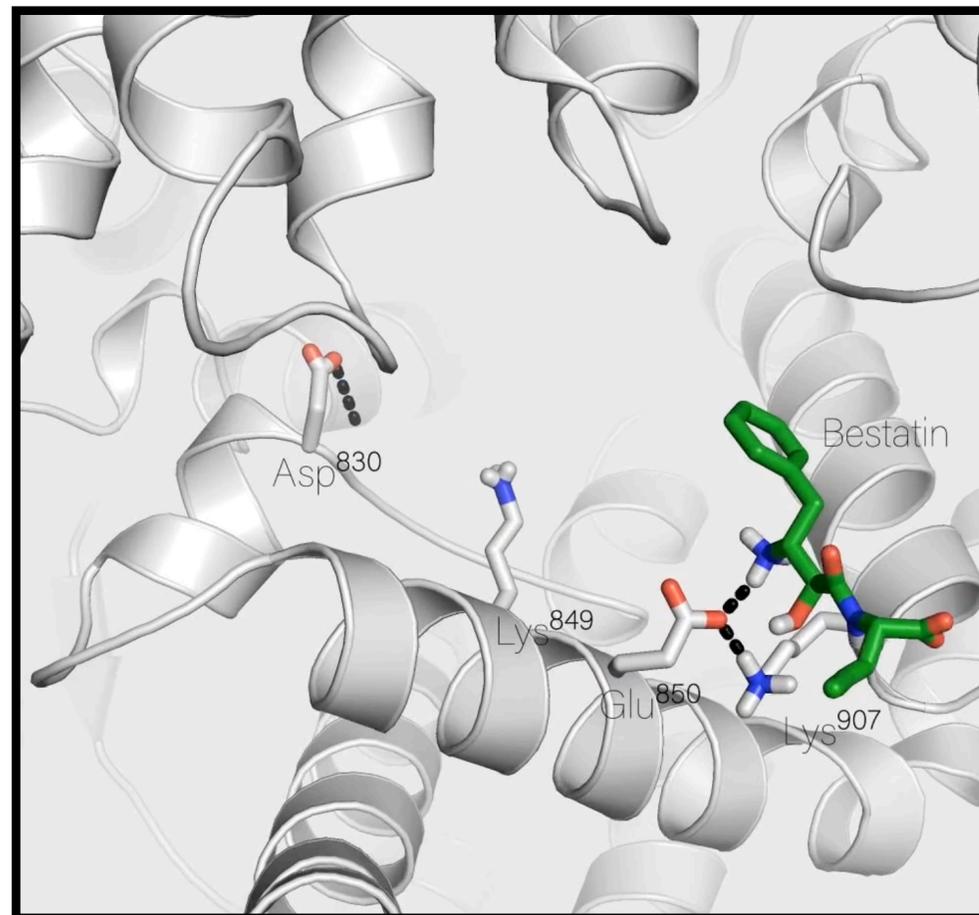
Rishwanth Raghu

COS598L, February 2026



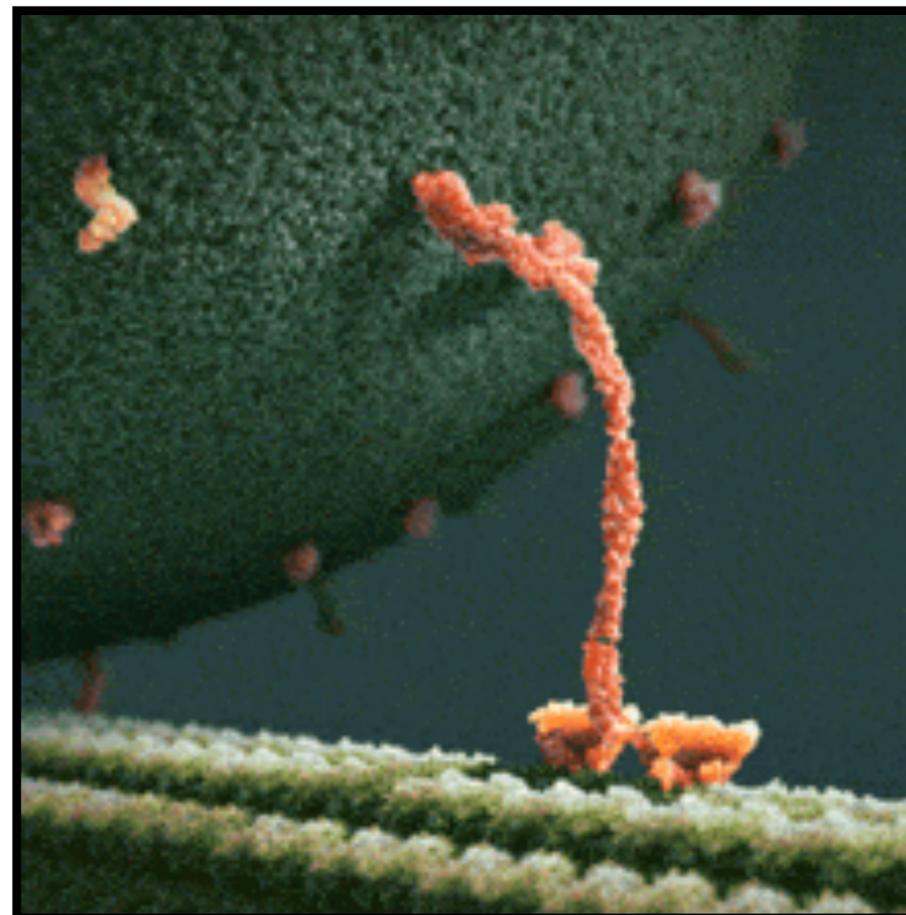
Protein structure and dynamics encode function across scales

M1 Aminopeptidase



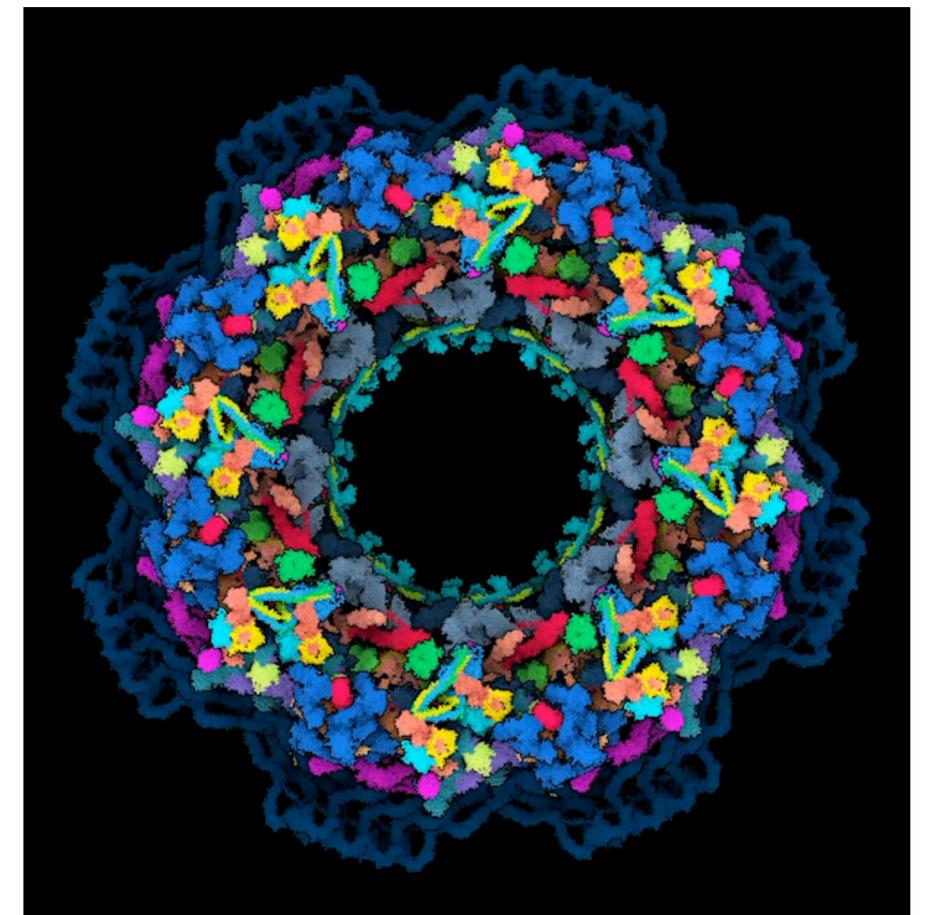
Moore et al. PLOS Comp Bio 2018

Dynein



Art of the Cell

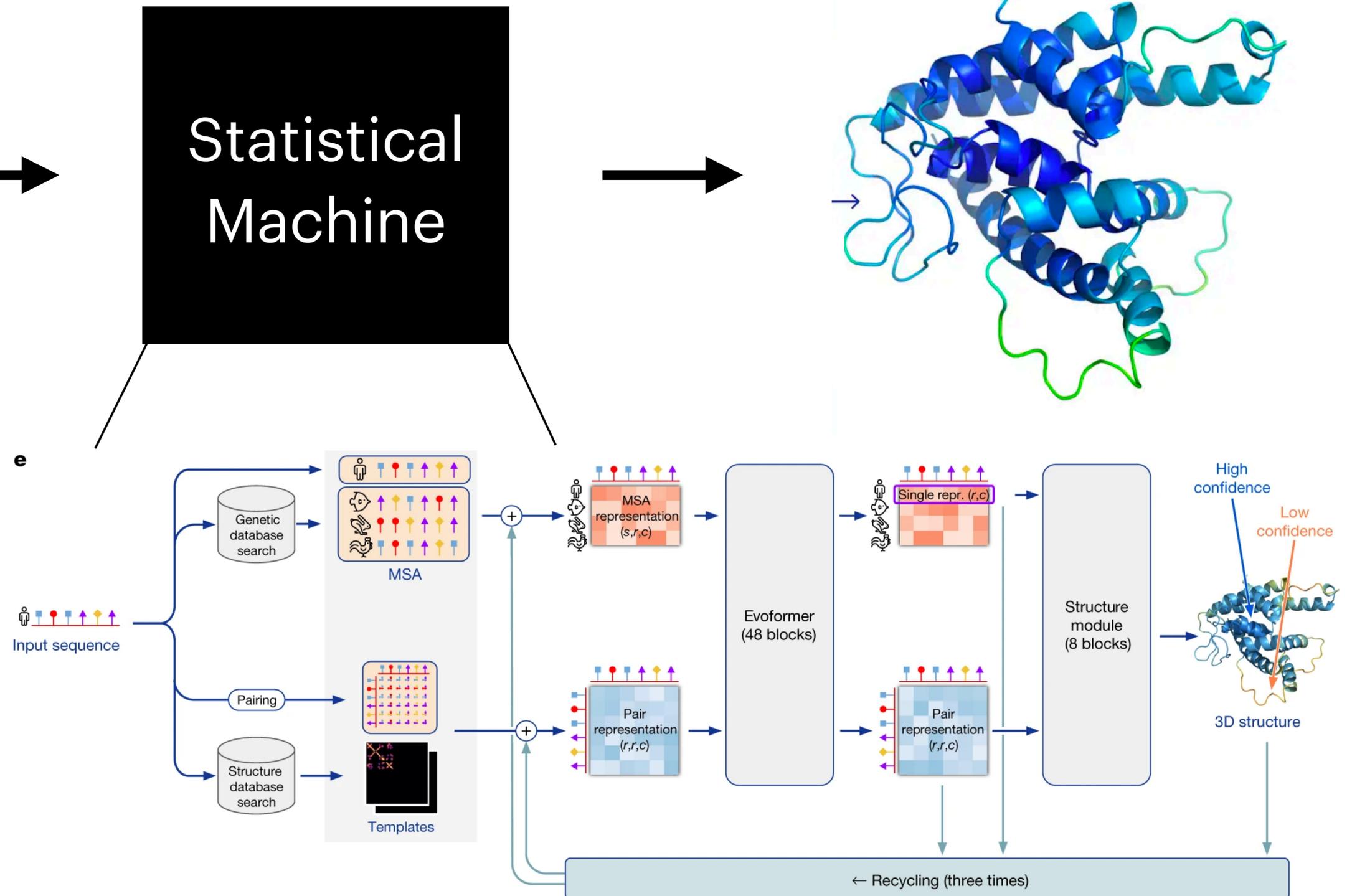
Nuclear Pore Complex



Mosalaganti et al. Science 2022

Protein Structure Prediction: AlphaFold

- Input sequence
MRKPRTPFTT...
- Sequence-to-structure prediction
- MSA encoding + structure decoding
- Trained on structures from Protein Data Bank

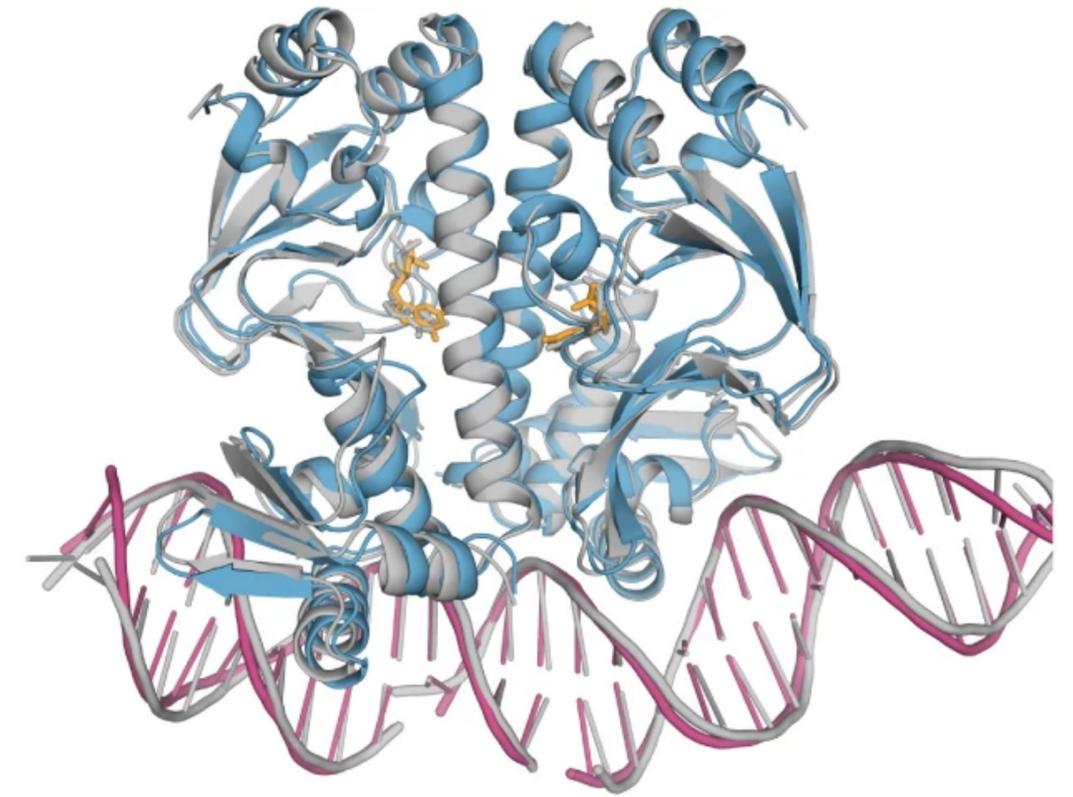


Protein Structure Prediction: AlphaFold

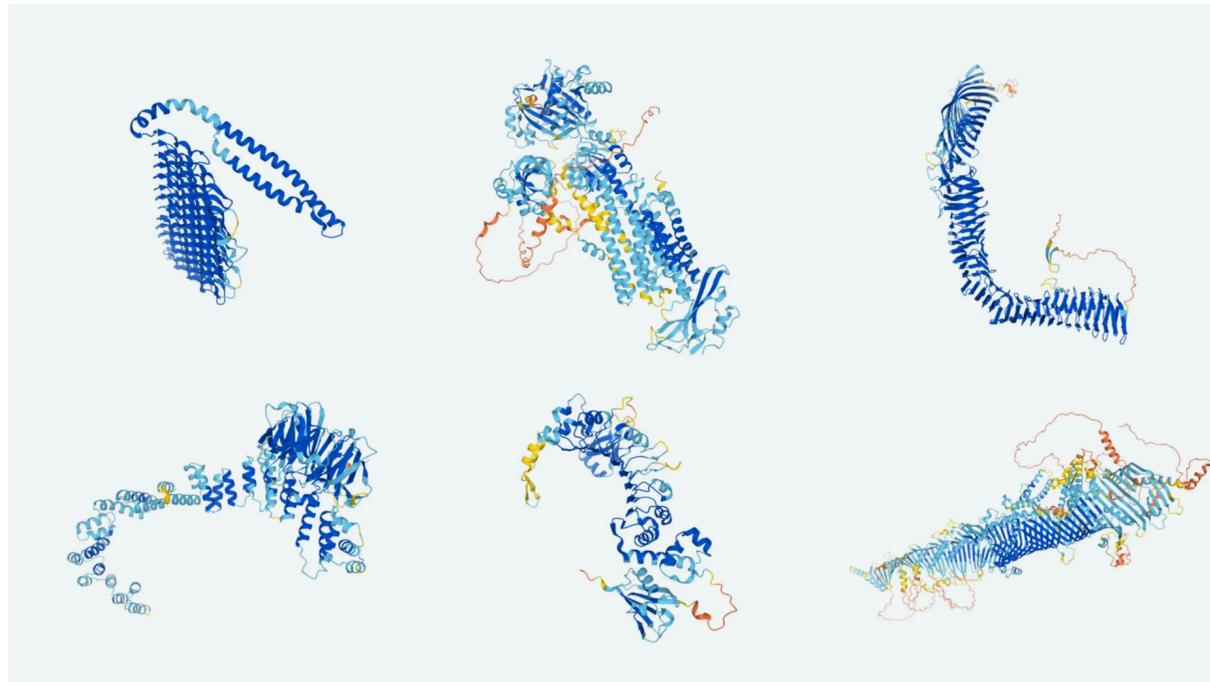
Median Free-Modelling Accuracy



92.4 GDT @ CASP
(Within experimental error)



AF3 modeling of proteins, nucleic acids, and ligands



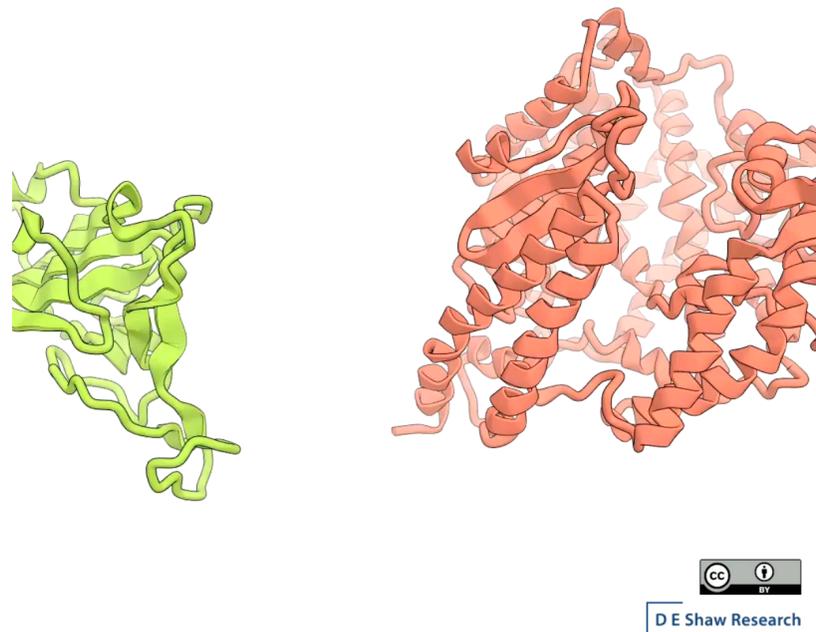
>214 million predicted structures in AFDB

Did AlphaFold “solve” the protein structure prediction problem?

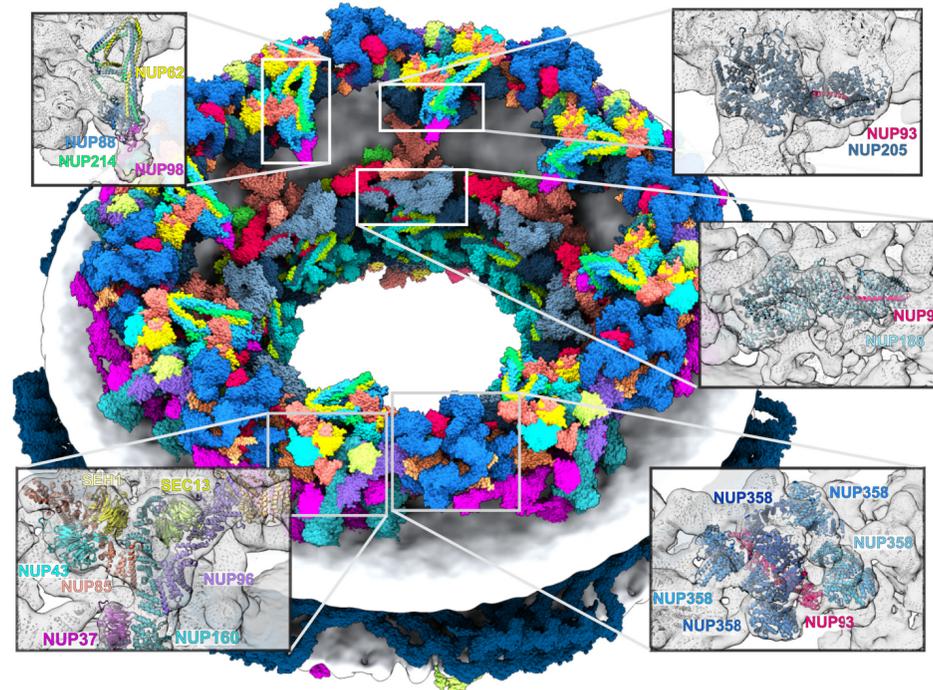
What is the role of structure *determination*?

- AlphaFold provides valuable hypotheses, but experiment remains the best form of structure validation in biological discovery
- AlphaFold has limitations in predicting structures that are dynamic, large, or have few sequence homologs
- Experiment is the source of “ground truth” for training ML models

trajectory000151



Molecular dynamics simulation. DE Shaw Research.



Nuclear pore supercomplex. Mosalaganti et al.

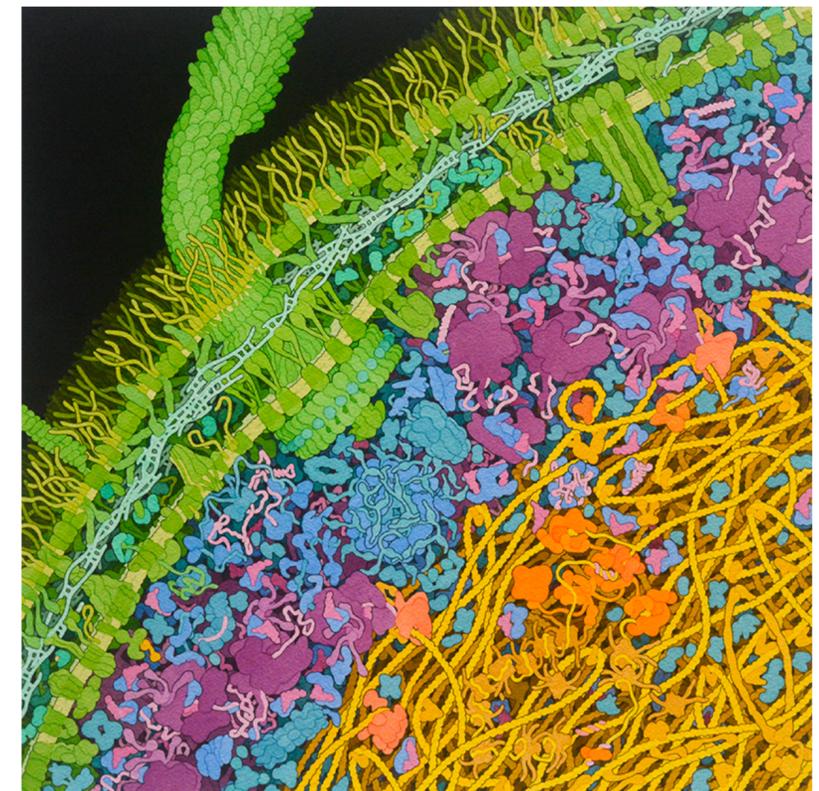
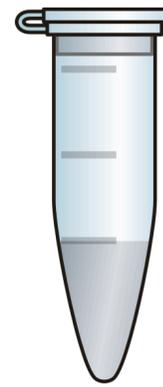
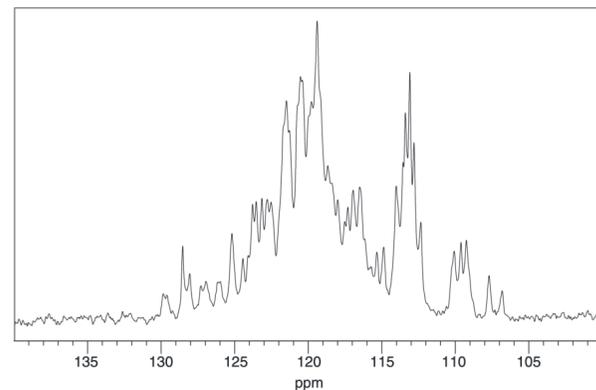
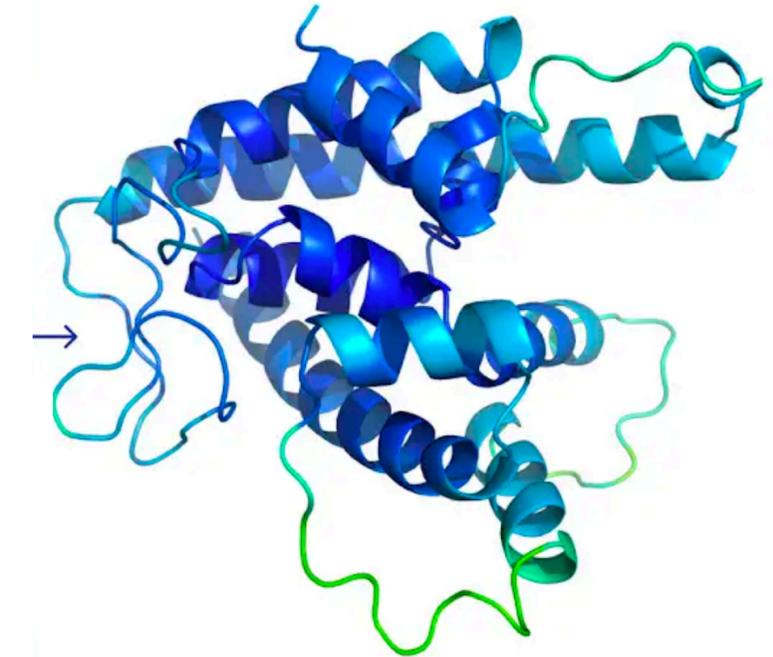


Illustration of the *E. coli* bacterium. David S Goodsell.

Protein Structure Determination

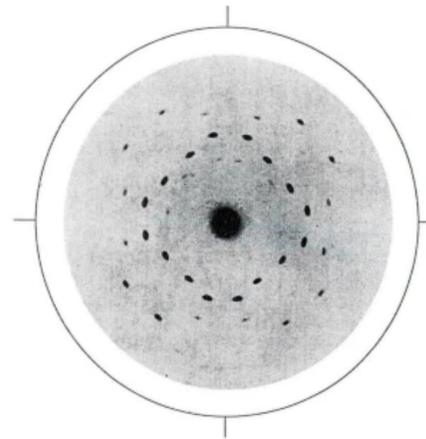


Protein sample



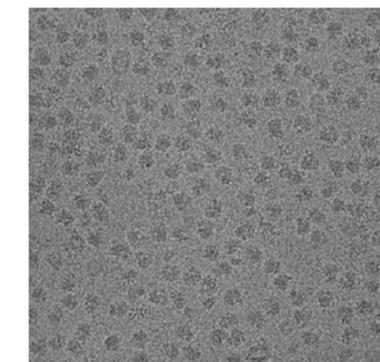
NMR

Solution state
Limited to smaller proteins



Crystallography

High resolution
Requires crystallization

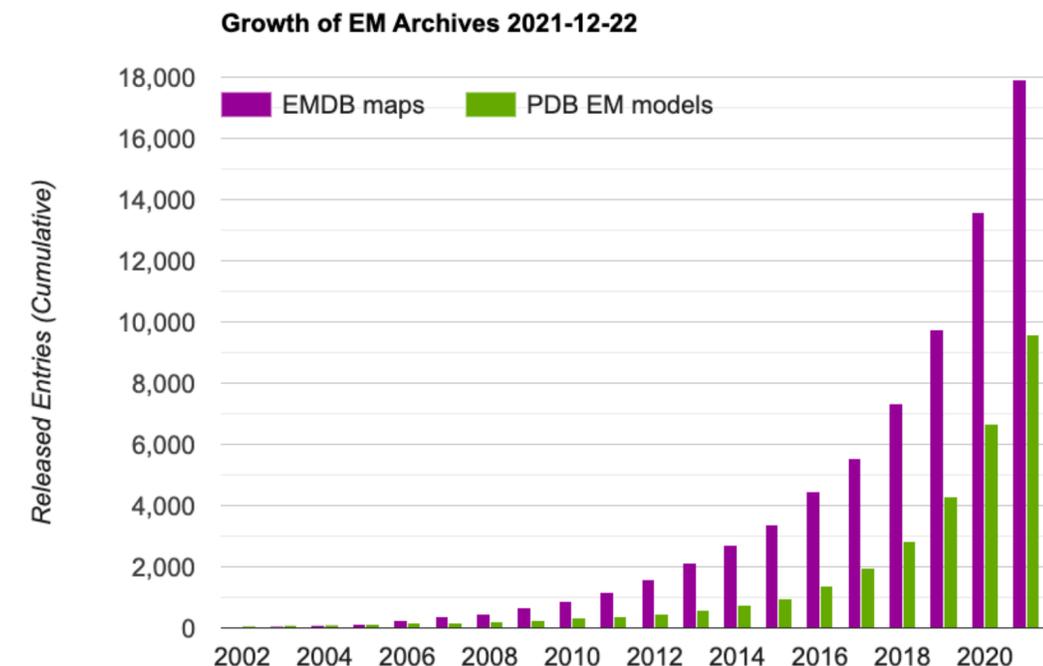
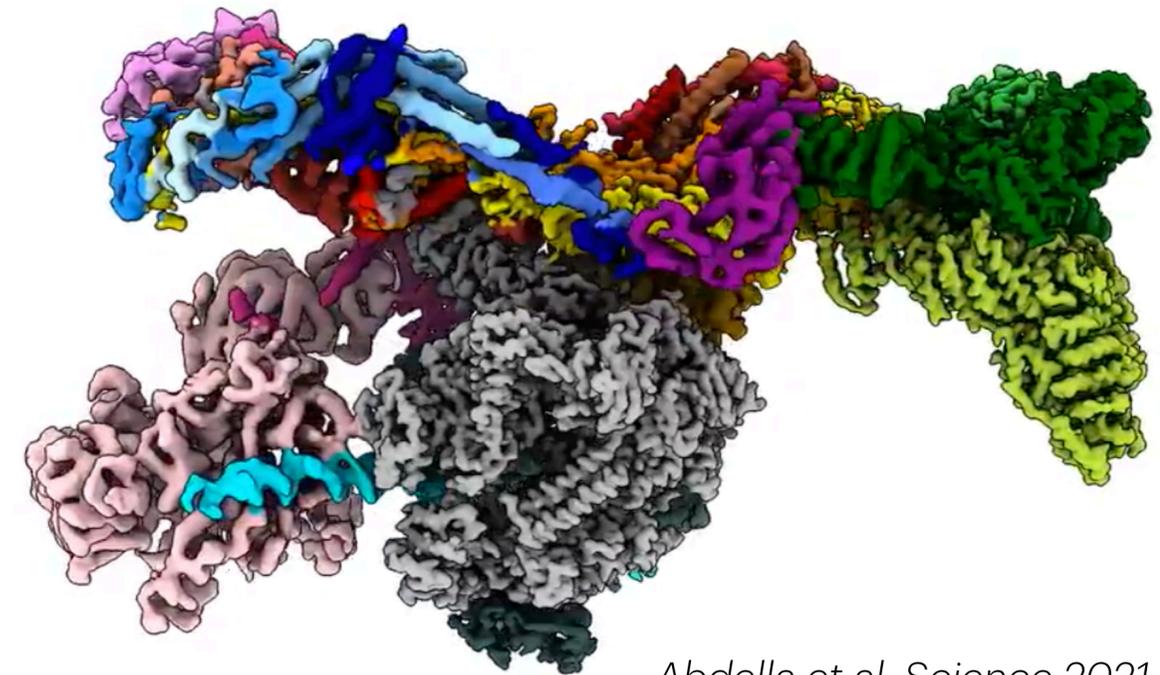


Cryo-EM

Captures dynamics
Limited to larger proteins

The ongoing cryo-EM “resolution revolution”

- 2017 Nobel Prize in Chemistry
- Cryo-EM has opened up new areas of structural biology
- Recent hardware and software breakthroughs:
 - **Hardware:** Direct electron detectors
 - **Software:** New reconstruction algorithms, GPU compute
 - **Faster:** Automation and democratization of cryo-EM imaging
- New computational challenges and opportunities



Roadmap

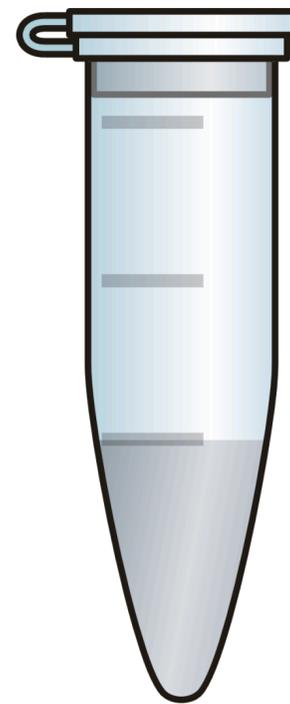
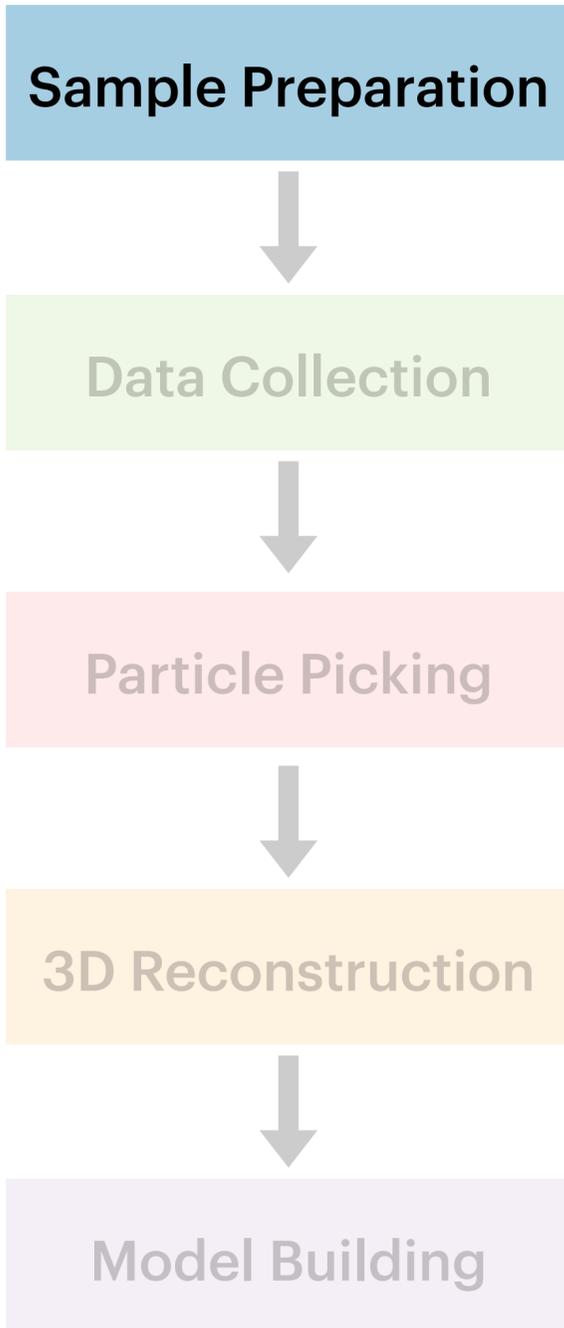
- Overview of the cryo-EM pipeline
- Classical cryo-EM reconstruction
 - Homogeneous reconstruction
 - Multiclass reconstruction
- Modern heterogeneous reconstruction
 - CryoDRGN

Roadmap

- **Overview of the cryo-EM pipeline**
- Classical cryo-EM reconstruction
 - Homogeneous reconstruction
 - Multiclass reconstruction
- Modern heterogeneous reconstruction
 - CryoDRGN

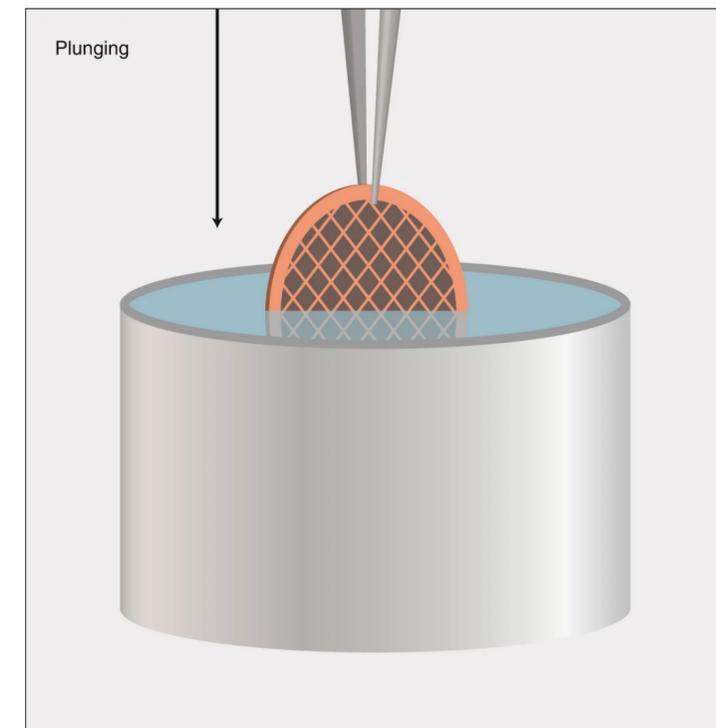
Sample Preparation

- The protein of interest is purified and flash frozen into a thin specimen
- ▶ Freezing traps molecules in place, and increases radiation tolerance
 - ▶ More proteins are amenable to freezing than crystallization
 - ▶ Molecules are sampled from an "equilibrium" distribution of conformations



Purified Protein

Vitrification →



Cryo-EM Sample

Data Collection

The sample is irradiated with electrons to produce 2D projection data of electron scattering potential

Sample Preparation



Data Collection



Particle Picking



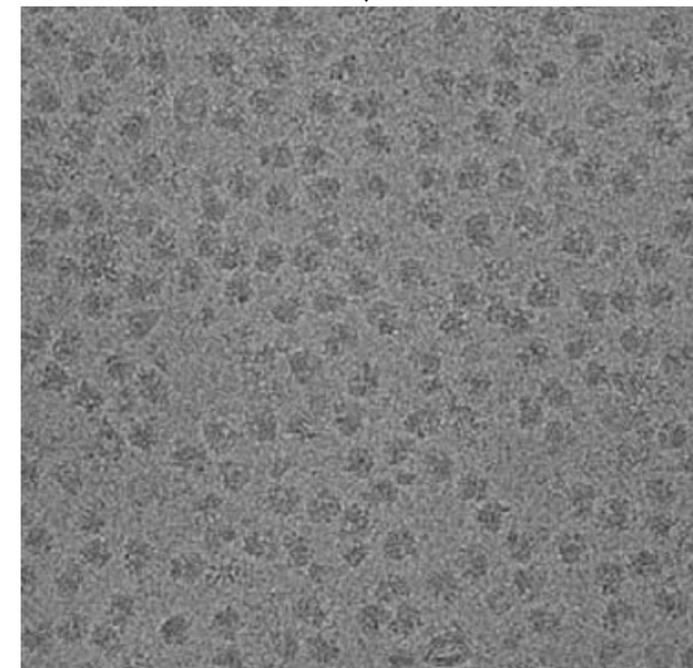
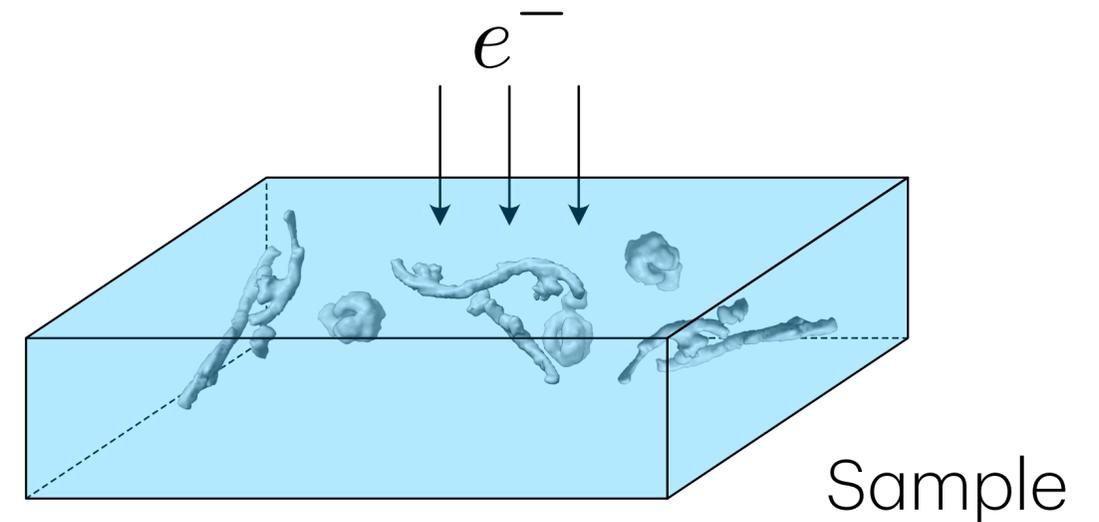
3D Reconstruction



Model Building



Laboratory of Biological Electron Microscopy

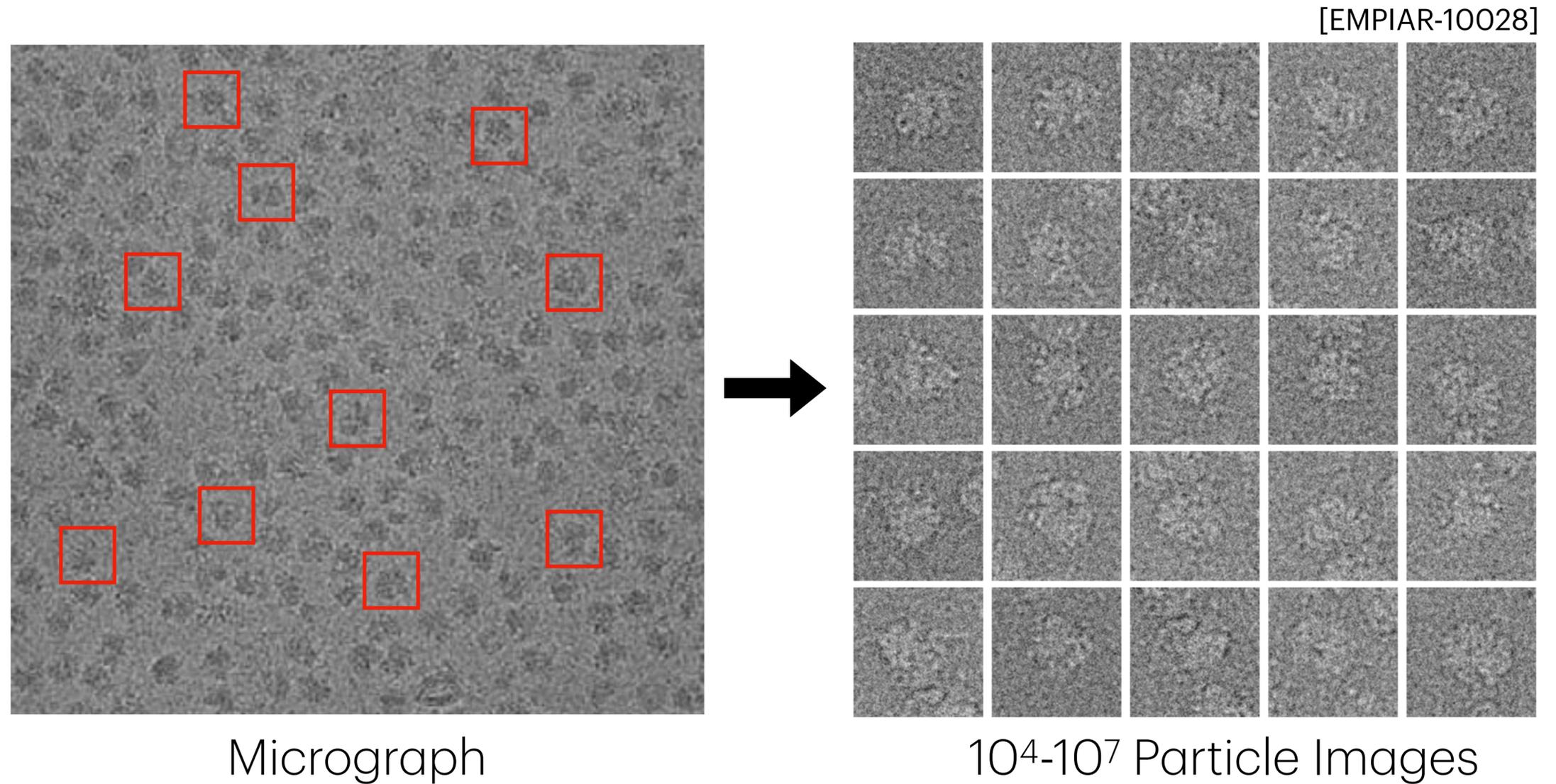
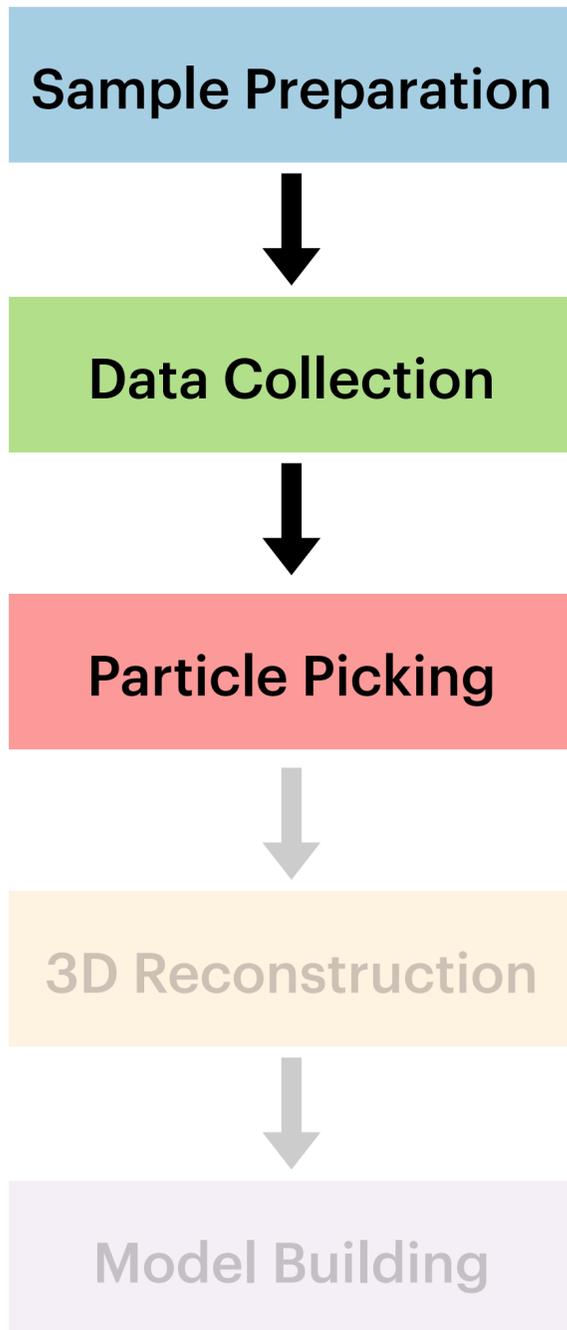


Micrograph

[EMPIAR-10028]

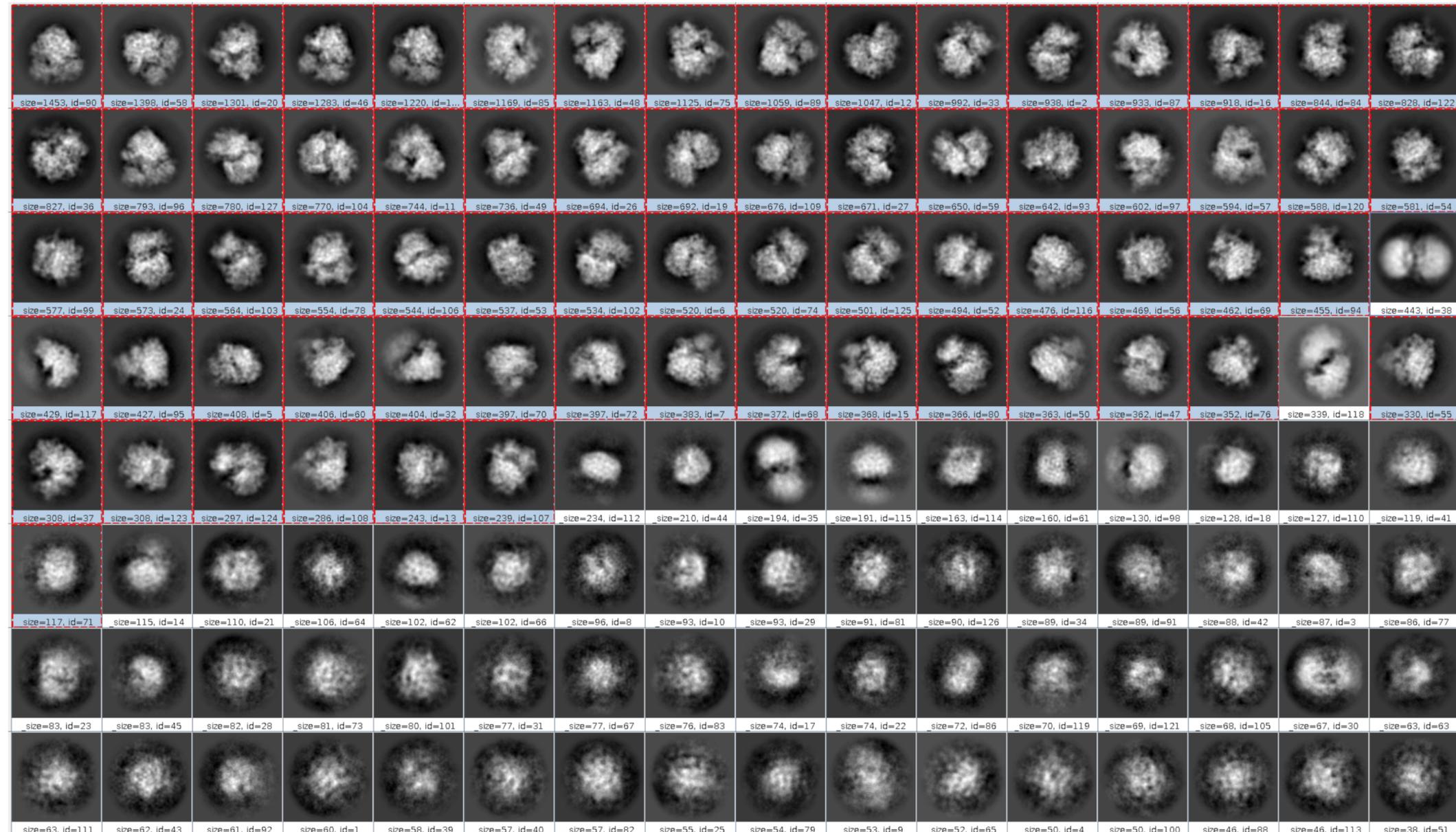
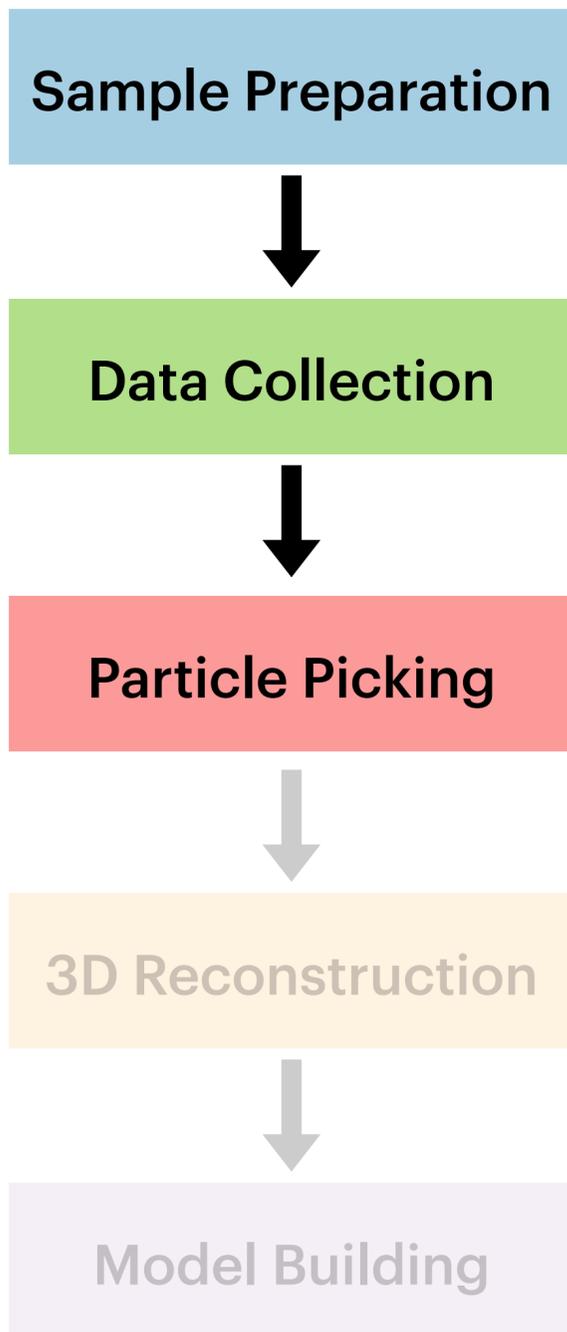
Particle Picking

Individual particles are extracted from micrographs using manual selection, machine learning methods, or prior structural templates



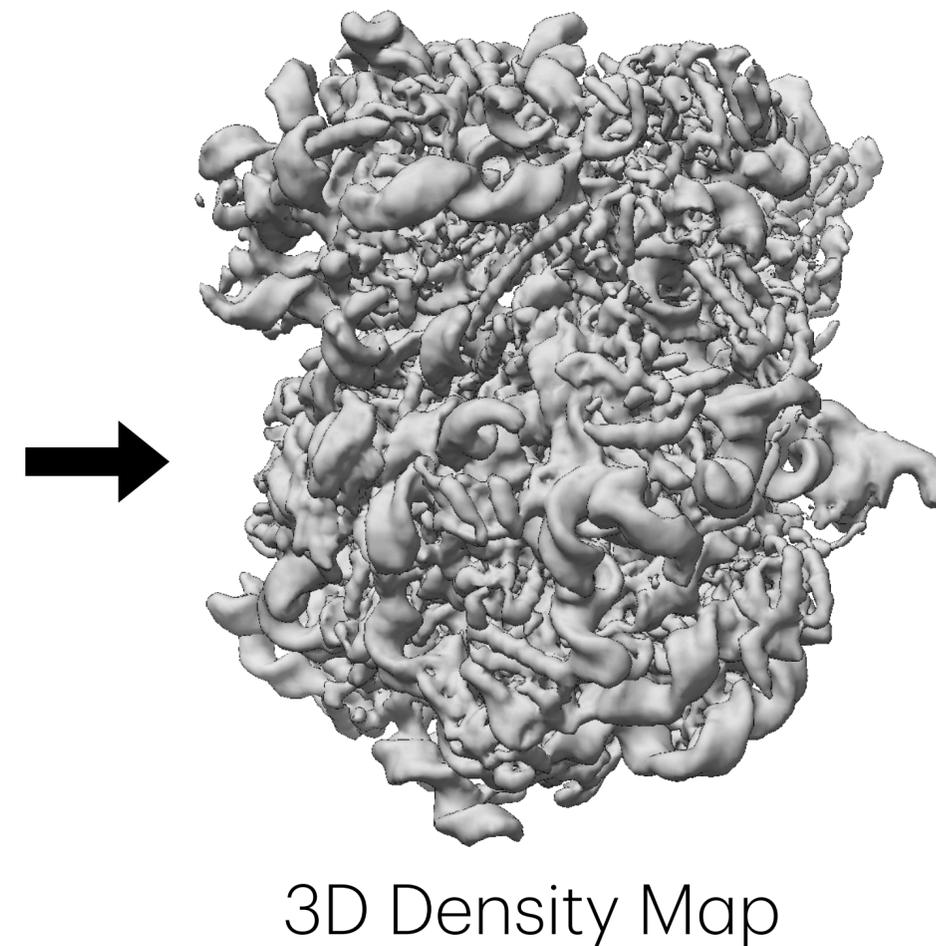
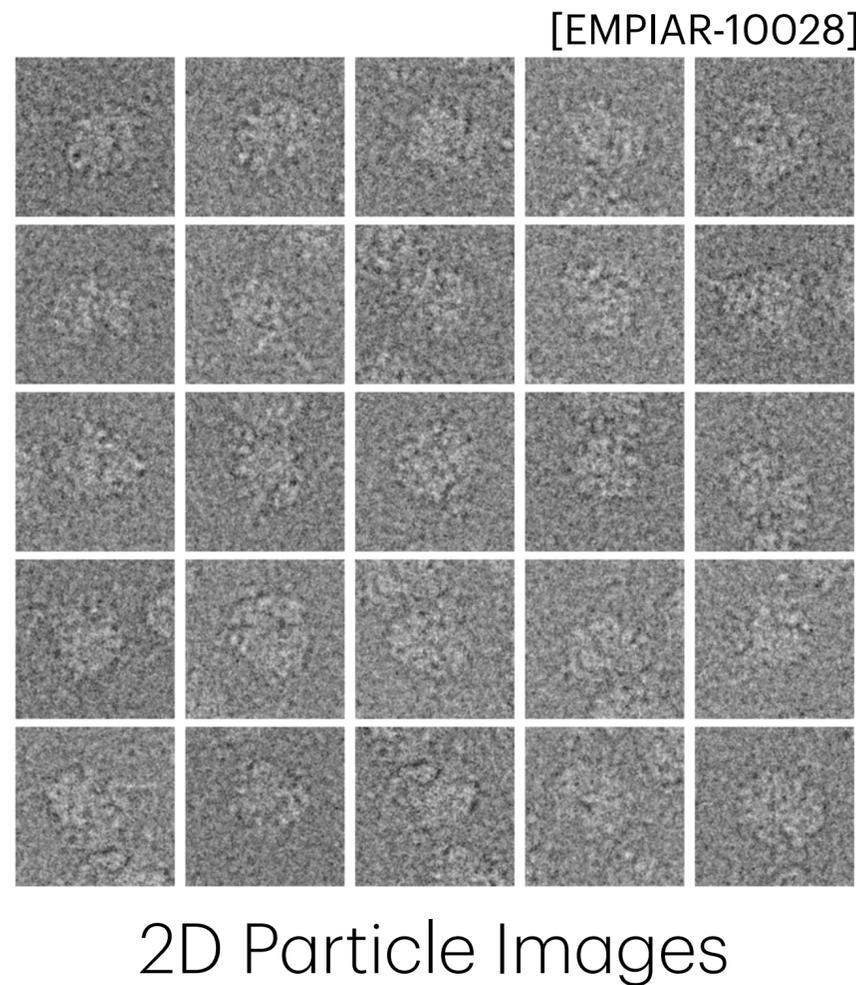
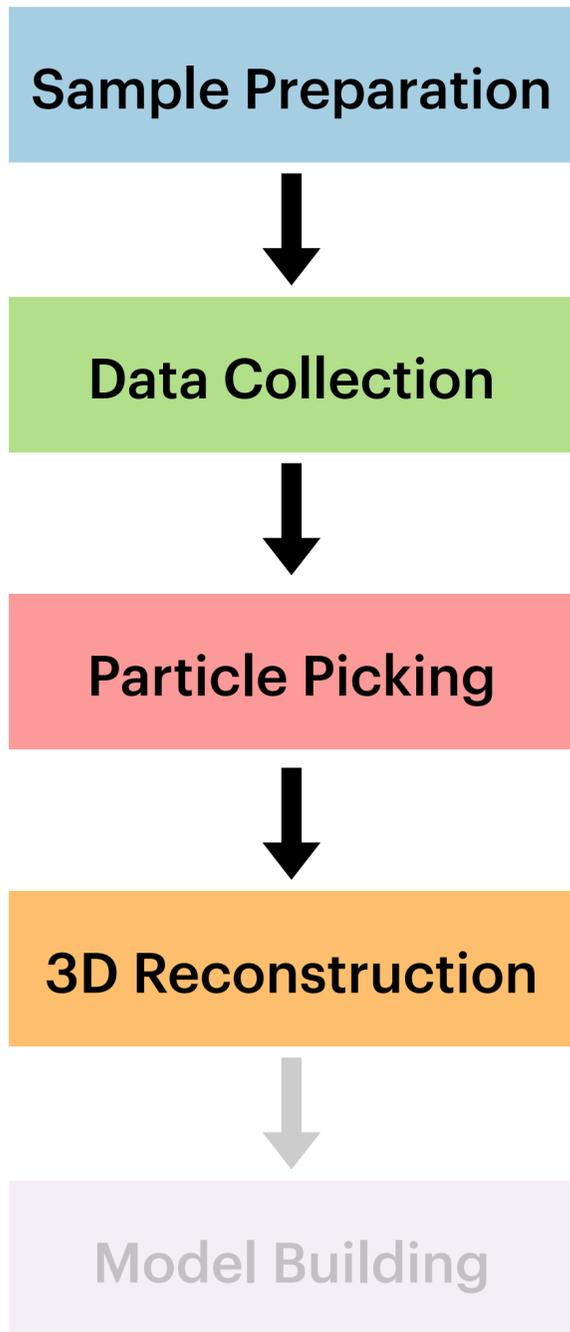
2D Classification

Cryo-EM datasets often contain junk or outlier particles, which may be filtered out by selecting good classes of averaged particles



3D Reconstruction

The noisy 2D projection images are reconstructed into a 3D volume representing the protein's structure

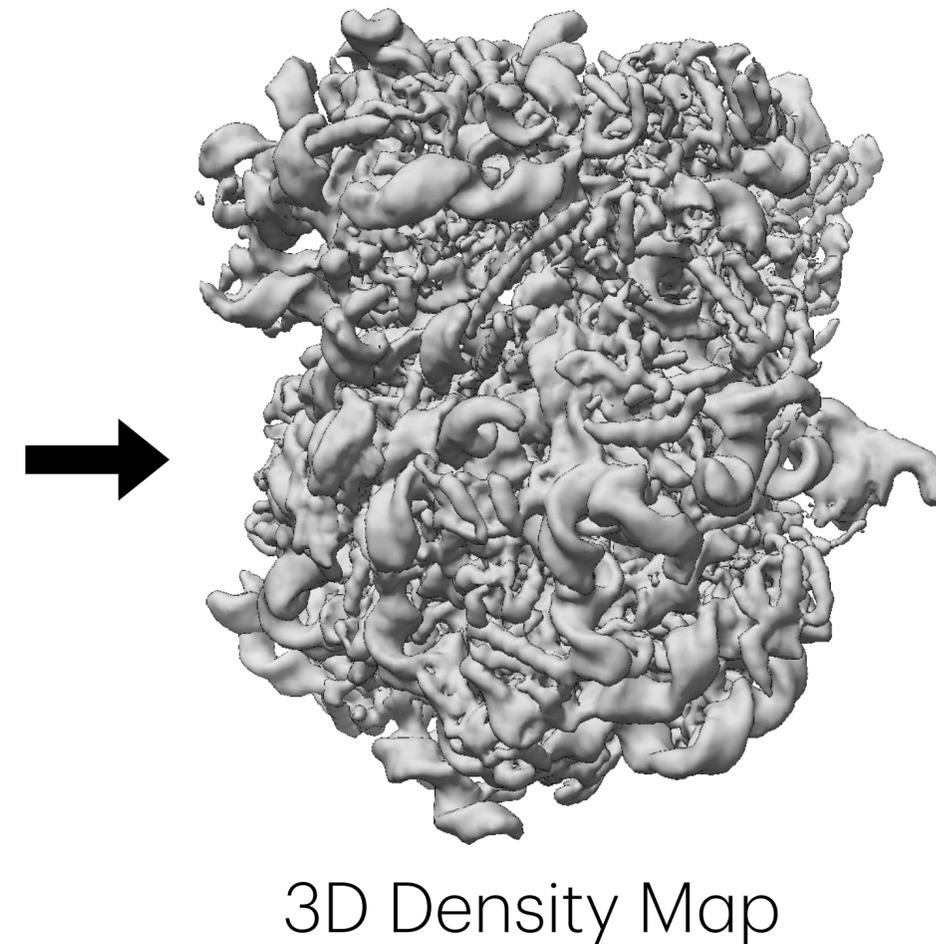
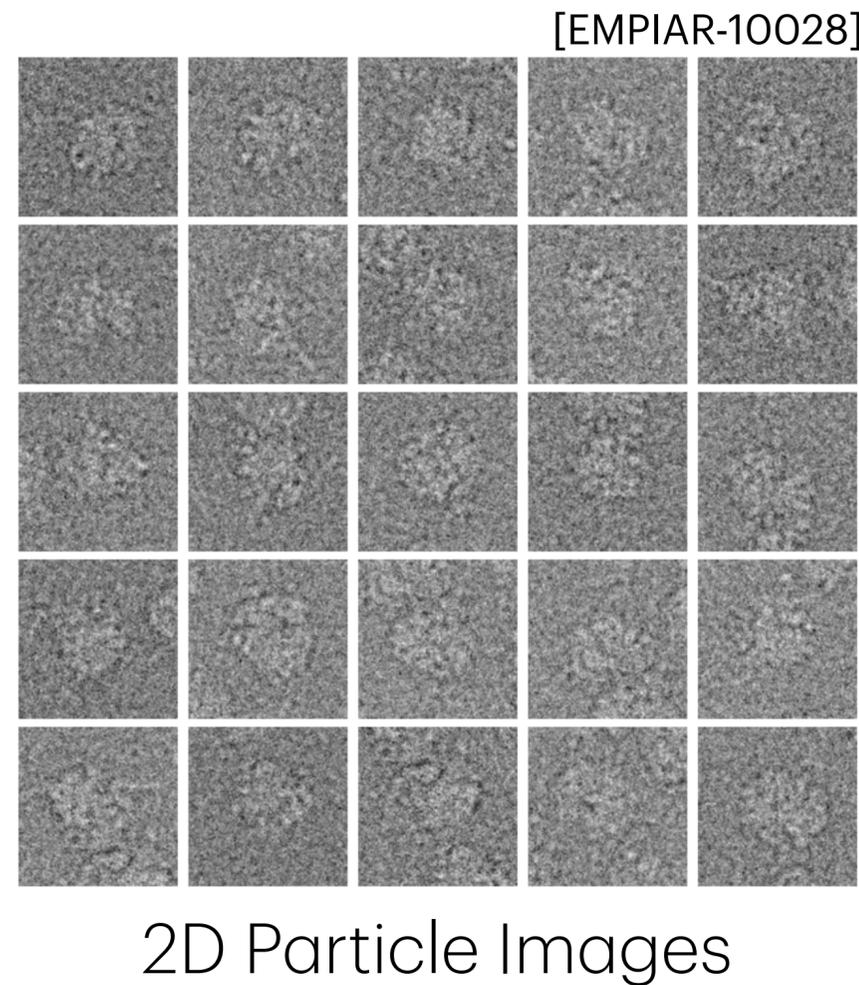
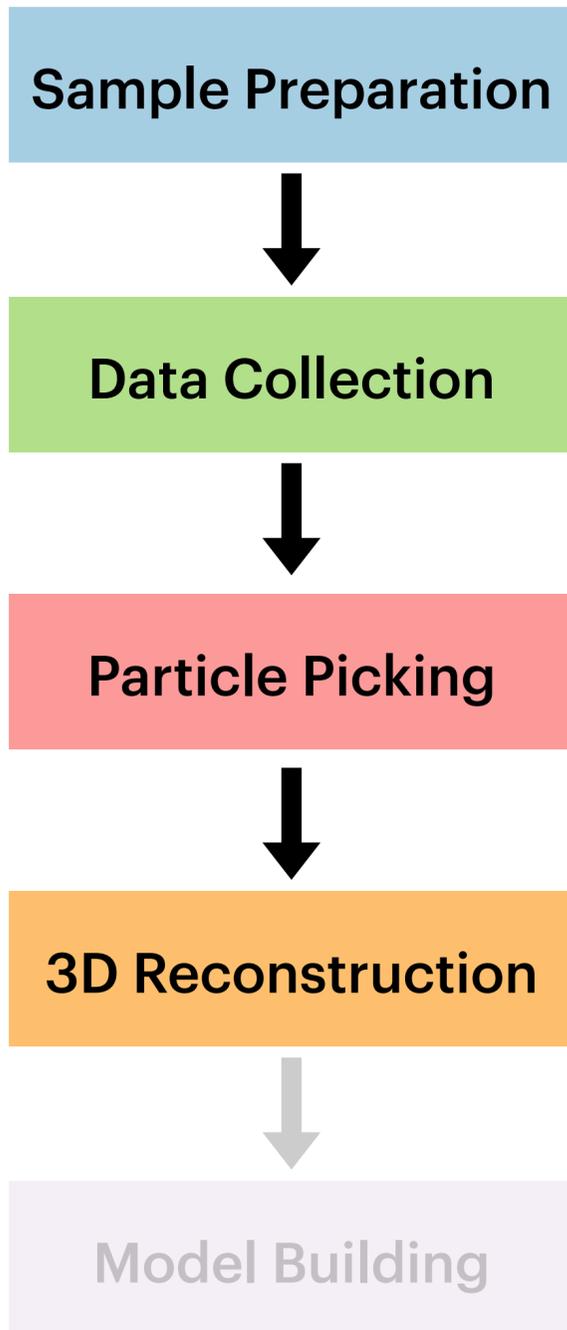


What makes 3D reconstruction challenging in cryo-EM?

Key principle: Biological samples are highly radiation-sensitive, but high-resolution structure can be recovered by combining information across thousands or millions of particles

3D Reconstruction

The noisy 2D projection images are reconstructed into a 3D volume representing the protein's structure



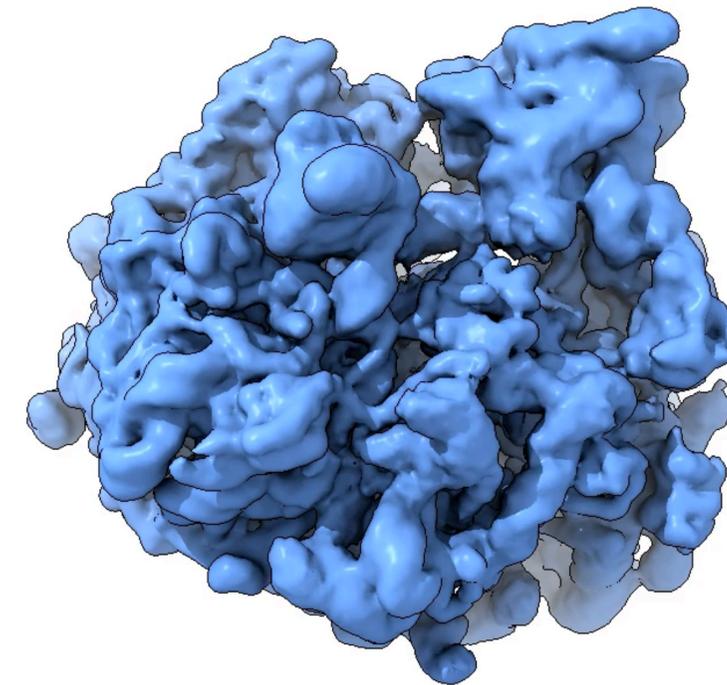
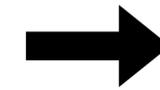
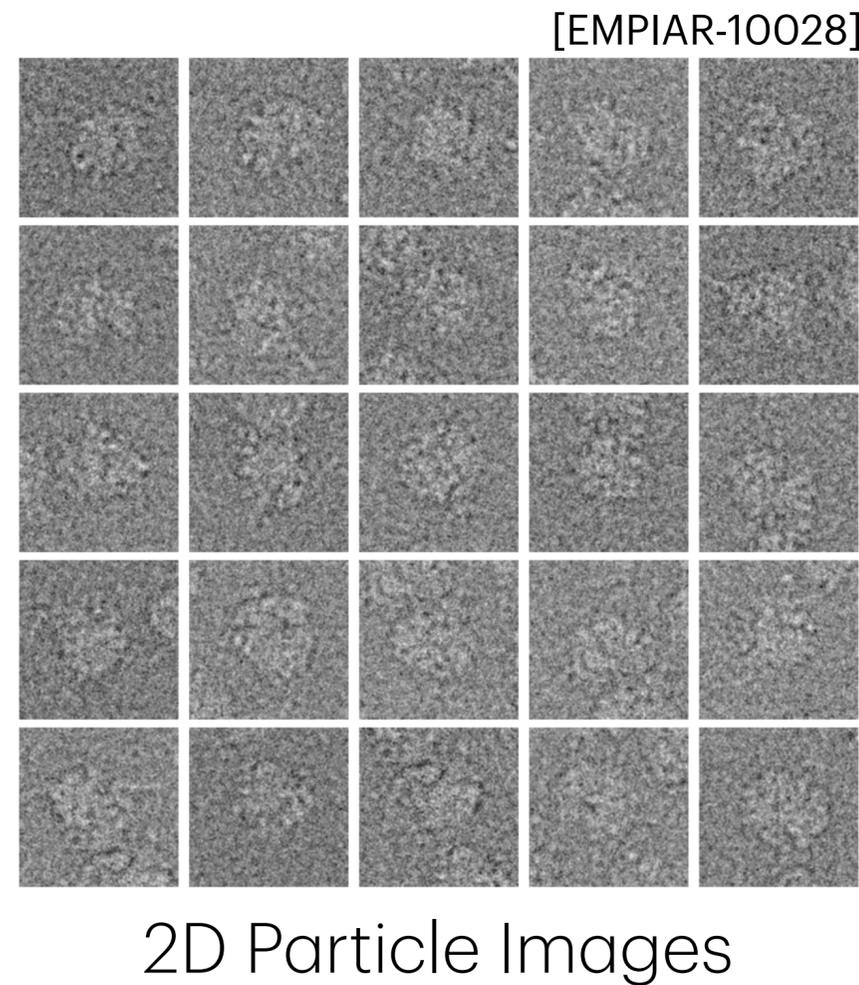
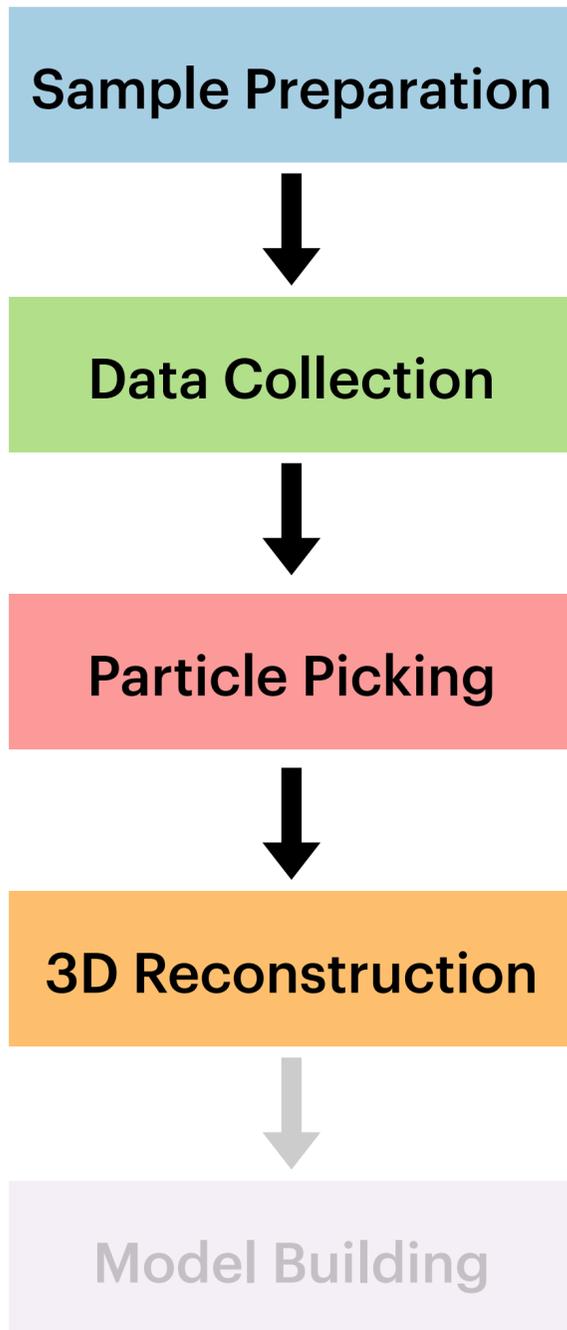
Challenges

- Unknown particle poses
- Low signal to noise ratio
- Microscope aberrations

Key principle: Biological samples are highly radiation-sensitive, but high-resolution structure can be recovered by combining information across thousands or millions of particles

3D Reconstruction

As each image arises from a unique particle, several 3D volumes may be reconstructed as well, representing the protein's dynamic structure



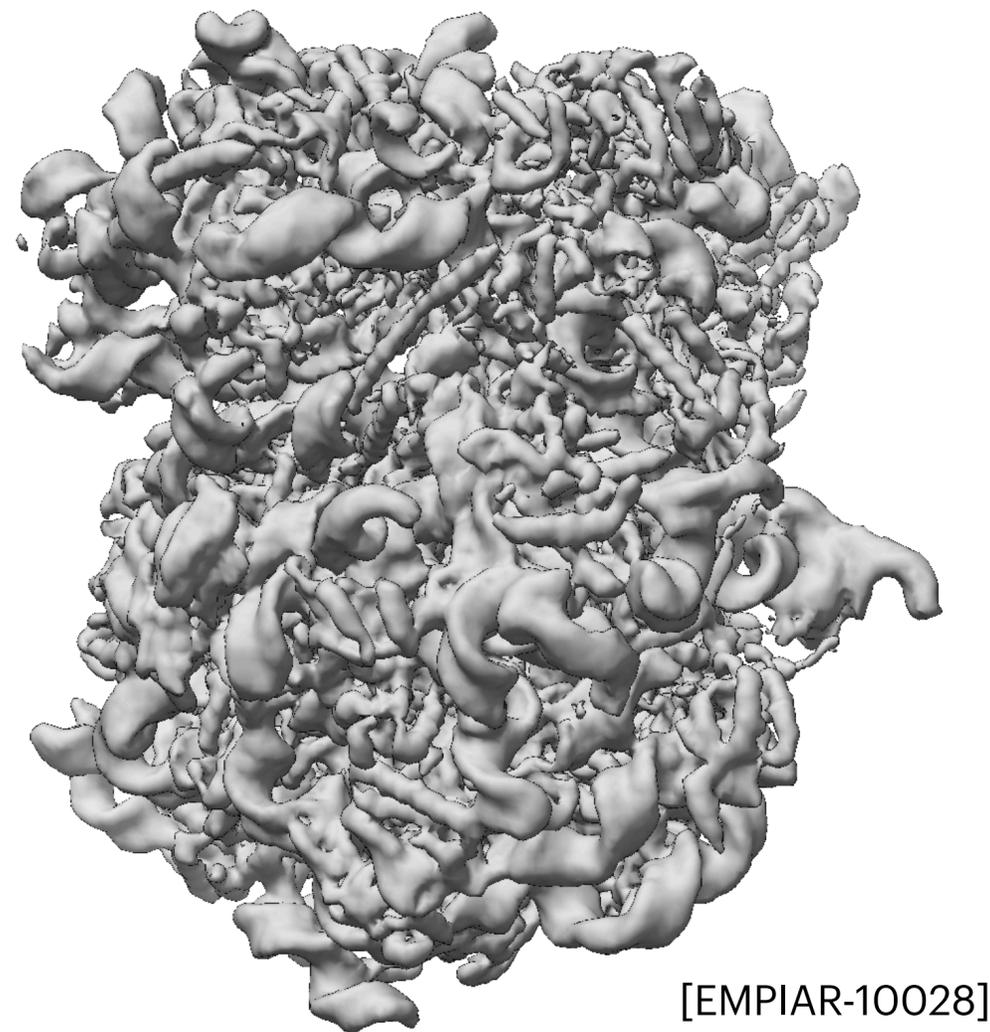
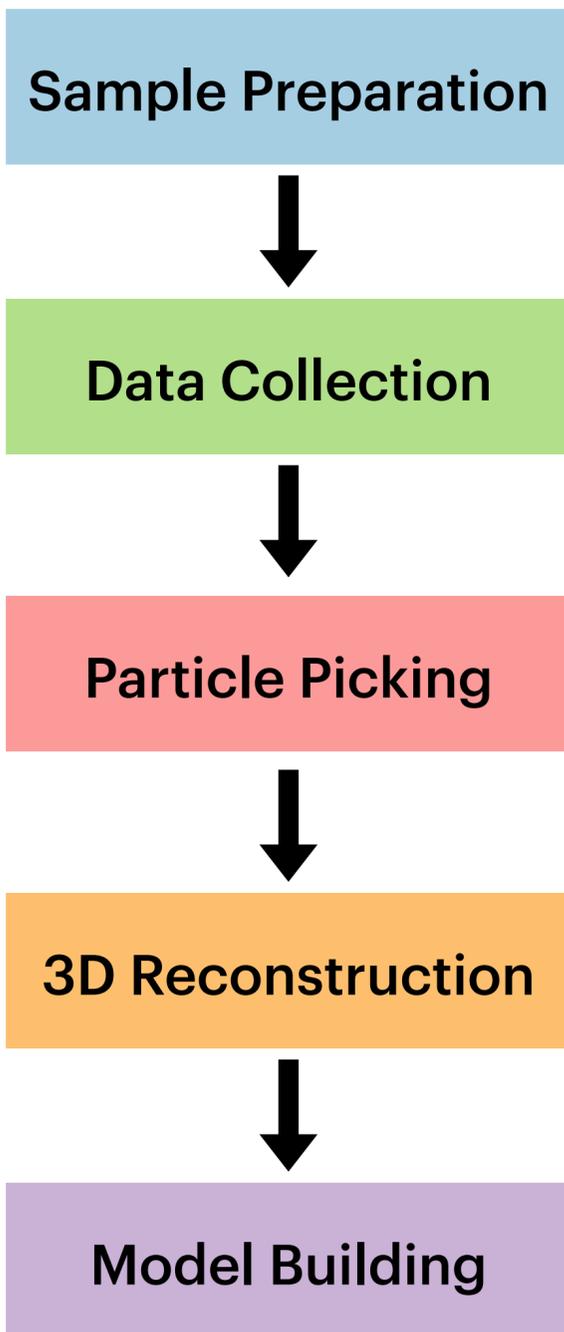
3D Density Maps

Challenges

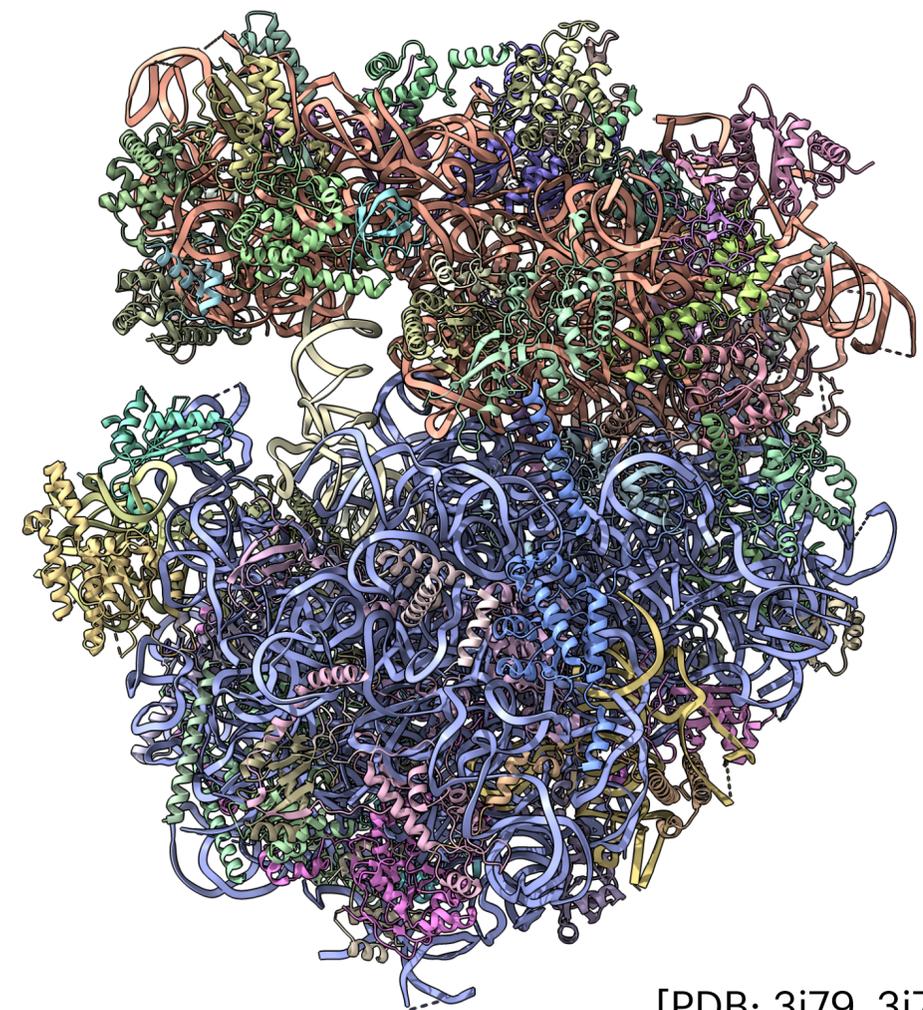
- Unknown particle poses
- Low signal to noise ratio
- Microscope aberrations
- **Structural heterogeneity**

Model Building

Amino acid identities and positions can be fit into high-resolution cryo-EM density maps to build atomic models



Cryo-EM Density Map



Atomic Model

Roadmap

- Overview of the cryo-EM pipeline
- Classical cryo-EM reconstruction
 - **Homogeneous reconstruction**
 - Multiclass reconstruction
- Modern heterogeneous reconstruction
 - CryoDRGN

Cryo-EM Image Formation Model

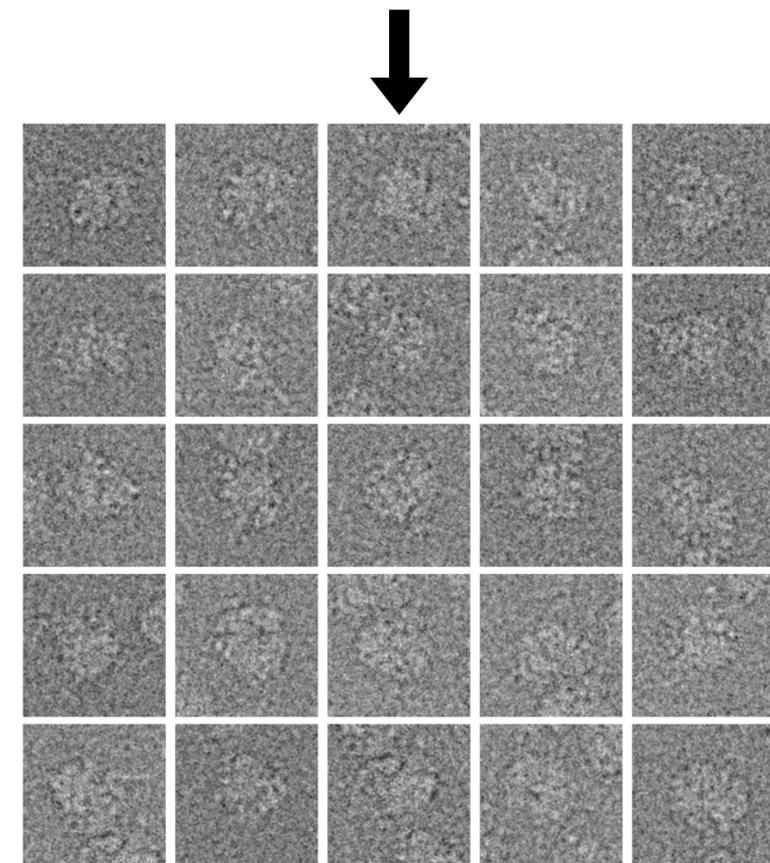
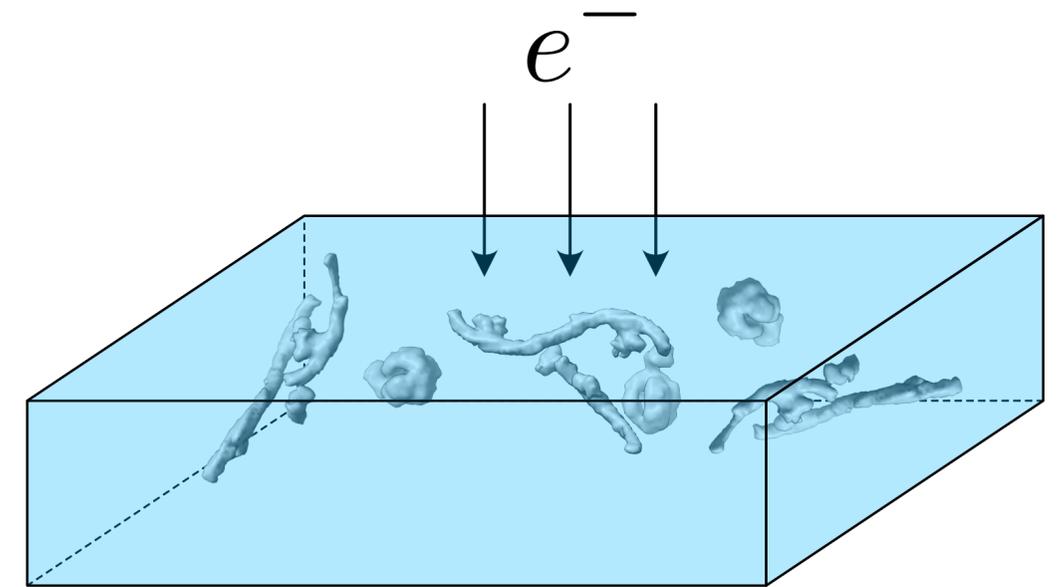
Image Formation Model

$$X_i = C_i * \mathcal{P}_{\phi_i} V + \eta_i$$

2D Image Contrast transfer function Projection about 5D pose 3D Cryo-EM density Gaussian noise $\mathcal{N}(0, \sigma^2)$

5D pose:

- 3D rotation, due to random particle orientation within sample
- 2D translation, due to imperfect centering of particle within image



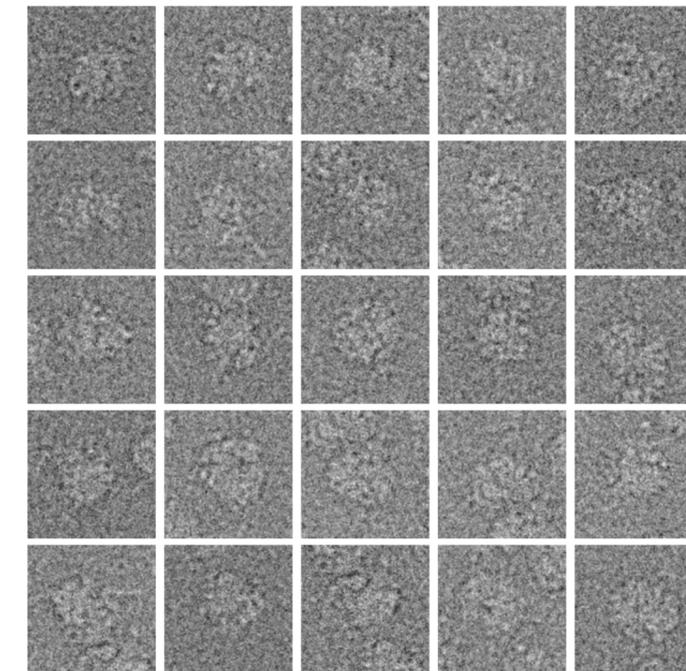
[EMPIAR-10028]

Cryo-EM Reconstruction Problem

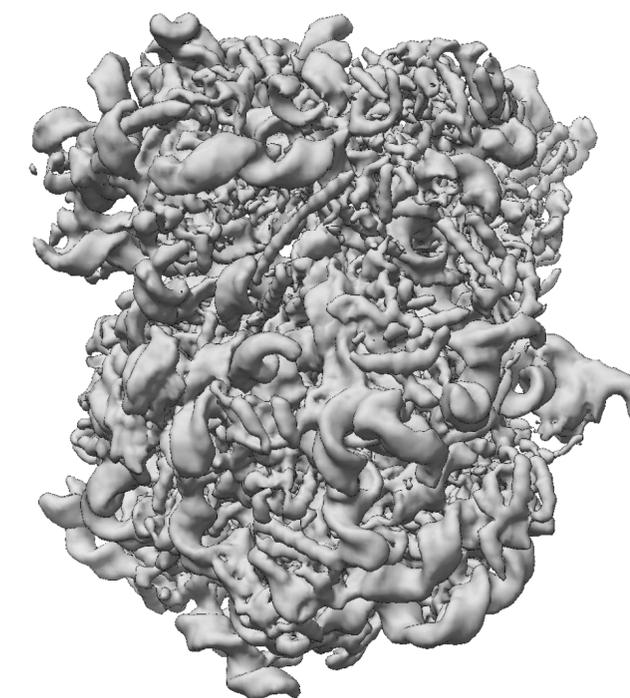
Image Formation Model

$$X_i = C_i * \mathcal{P}_{\phi_i} V + \eta_i$$

2D Image Contrast transfer function Projection about 5D pose 3D Cryo-EM density Gaussian noise $\mathcal{N}(0, \sigma^2)$



[EMPIAR-10028]



**Cryo-EM reconstruction problem:
Find optimal volume V given the data**

Assume CTF values C_i are known but poses ϕ_i are unknown

Maximum Likelihood Objective

Recall the image formation model:

$$X_i = C_i * \mathcal{P}_{\phi_i} V + \eta_i \implies X_i \sim \mathcal{N}(C_i * \mathcal{P}_{\phi_i} V, \sigma^2)$$

The likelihood of a single image (given volume and pose) is:

$$P(X_i | V, \phi) = \frac{1}{(2\pi\sigma^2)^{D^2/2}} \exp\left\{-\frac{\|X_i - C_i * \mathcal{P}_{\phi} V\|^2}{2\sigma^2}\right\} \quad D = \text{Image side length}$$

We seek the volume V that maximizes the log-likelihood over all images, marginalizing over poses:

$$\hat{V}^{\text{MLE}} = \arg \max_V \sum_{i=1}^n \log \int_{\text{SO}(3) \times \mathbb{R}^2} \exp\left\{-\frac{\|X_i - C_i * \mathcal{P}_{\phi} V\|^2}{2\sigma^2}\right\} d\phi$$

Maximize over volumes Sum over images Integrate over pose space Image likelihood given a pose

Expensive, non-convex

Expectation-Maximization for MLE

Instead of maximizing the marginalized log-likelihood, maximize the expected log-likelihood instead:

$$\mathbb{E}_{\phi_1, \dots, \phi_n} \left[\sum_{i=1}^n \log P(X_i | V, \phi_i) \right]$$

(E-Step) Update the posterior distribution of poses, given the current volume:

$$\forall i \in [n], s \in \mathcal{S} \quad w_i(s) = P(\phi_i = s | V^{(t)}, X_i) = \frac{P(X_i | V^{(t)}, \phi_i = s)}{\sum_{s' \in \mathcal{S}} P(X_i | V^{(t)}, \phi_i = s')}$$

Discretized candidate poses

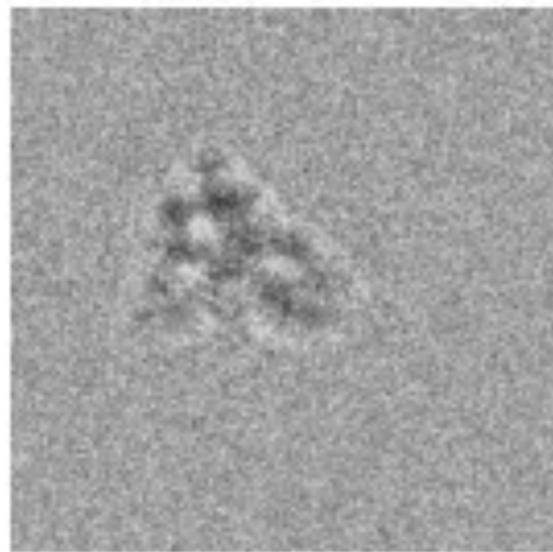
(M-Step) Update the volume, given the current pose posterior

$$V^{(t+1)} = \arg \min_V \sum_{i=1}^n \sum_{s \in \mathcal{S}} w_i(s) \|X_i - C_i * \mathcal{P}_s V\|^2$$

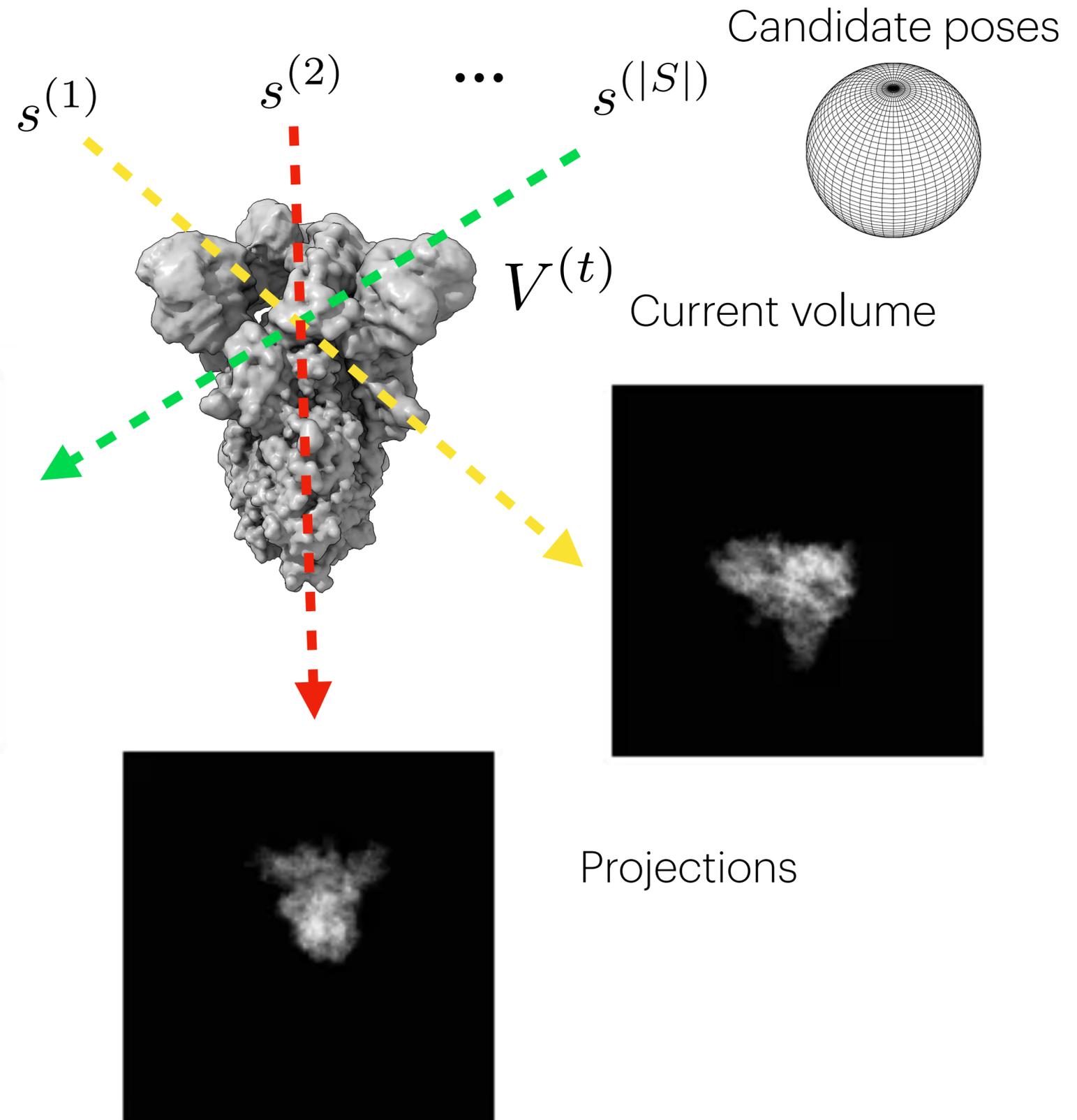
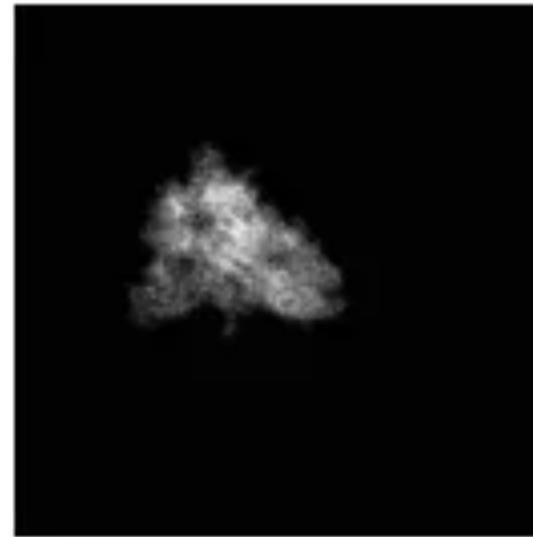
$$V^{(t+1)} = A^{-1} \left(\sum_{i=1}^n \sum_{s \in \mathcal{S}} w_i(s) \mathcal{P}_s^T C_i * X_i \right) \quad A = \sum_{i=1}^n \sum_{s \in \mathcal{S}} w_i(s) (\mathcal{P}_s)^T C_i * C_i * \mathcal{P}_s$$

E-Step: Weighted Projection Matching

$$V^{(t+1)} = \arg \min_V \sum_{i=1}^n \sum_{s \in \mathcal{S}} w_i(s) \underbrace{\|X_i - C_i * \mathcal{P}_s V\|^2}_{\text{Re-projection error}}$$



Re-projection error

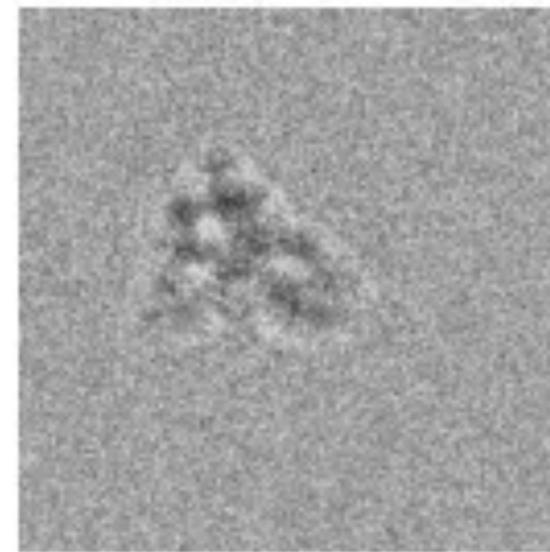


- If image is well-aligned, weights will be peaked
- If image pose is uncertain, weights will be more uniform, and contribute little to the reconstruction

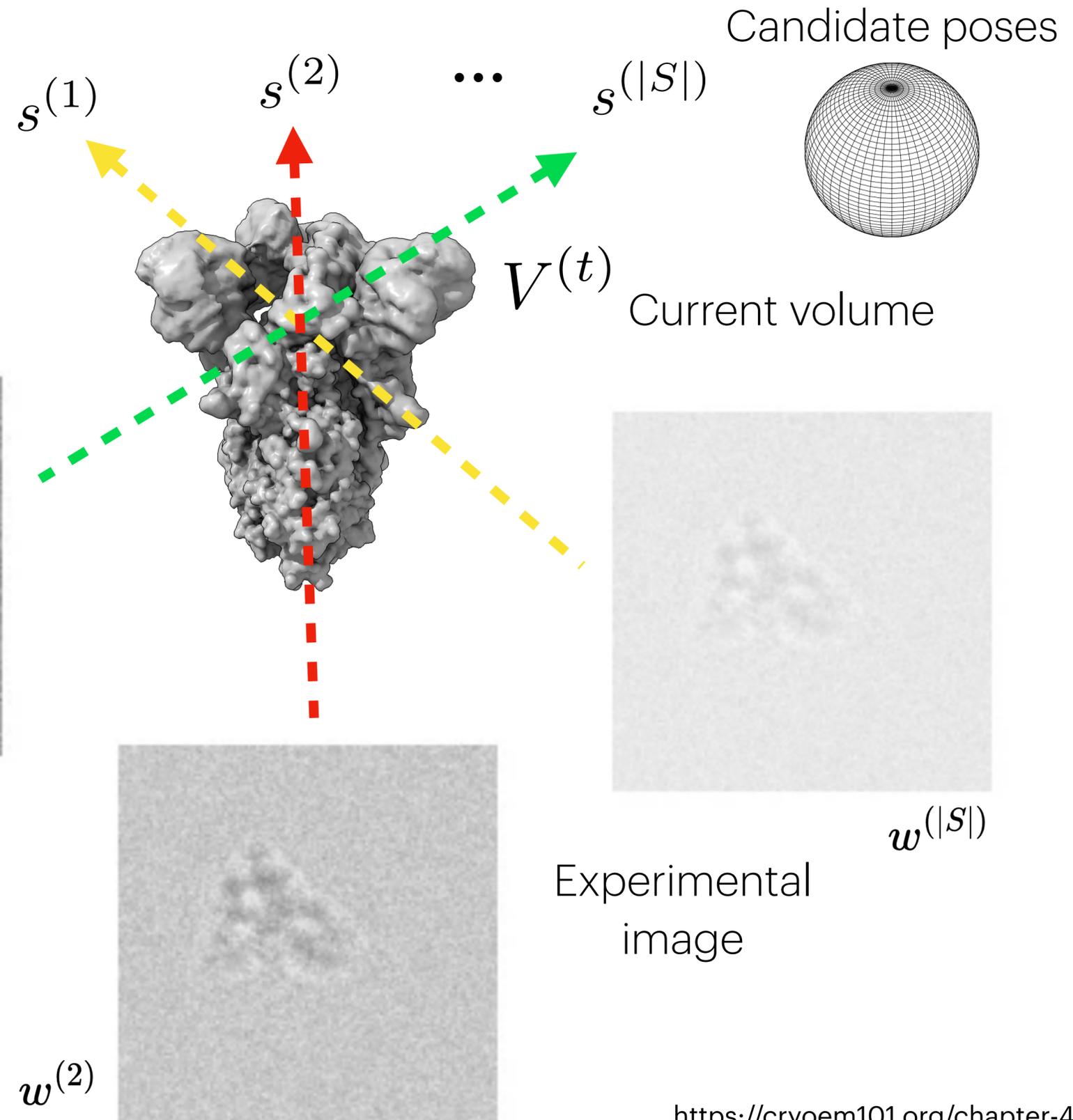
M-Step: Weighted Backprojection

$$V^{(t+1)} = A^{-1} \left(\sum_{i=1}^n \sum_{s \in S} w_i(s) \mathcal{P}_s^T C_i * X_i \right)$$

- “Inverse” projection of the original image at all candidate poses, using pose weights computed in E-step



$w^{(1)}$



Real vs Fourier Space

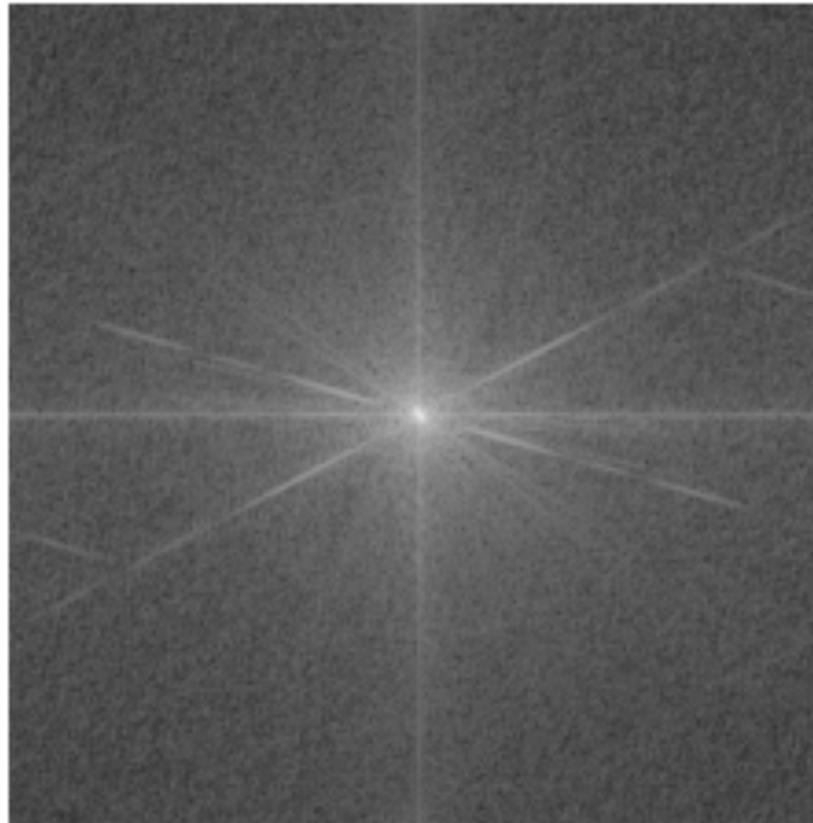
Image domain



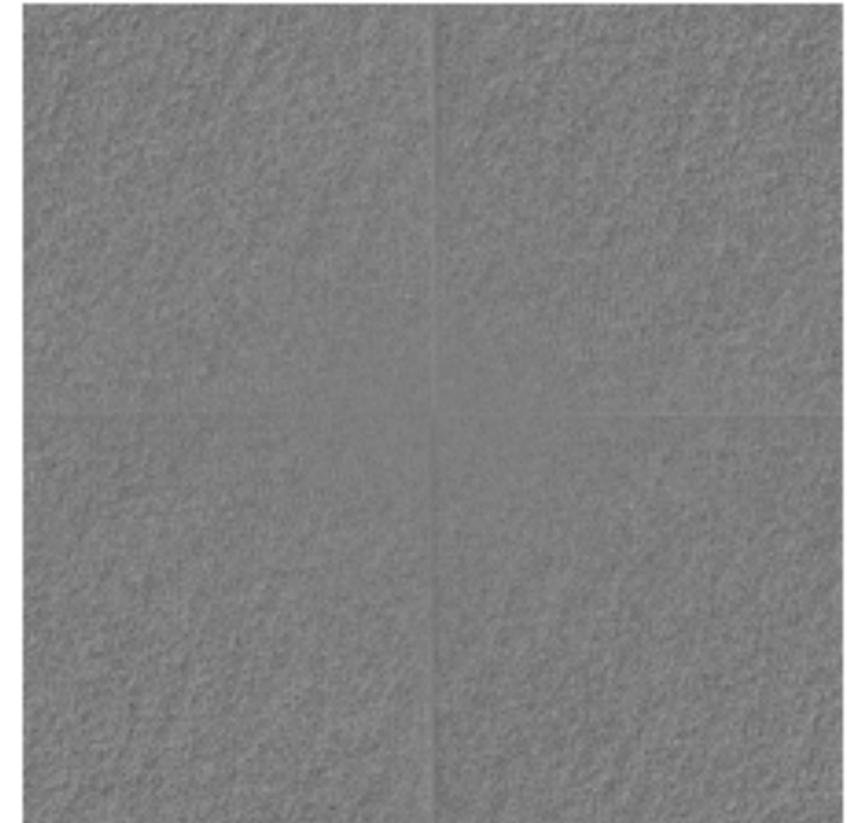
Real space

Intensity as a function of spatial coordinate

Magnitude of FFT



Phase of FFT

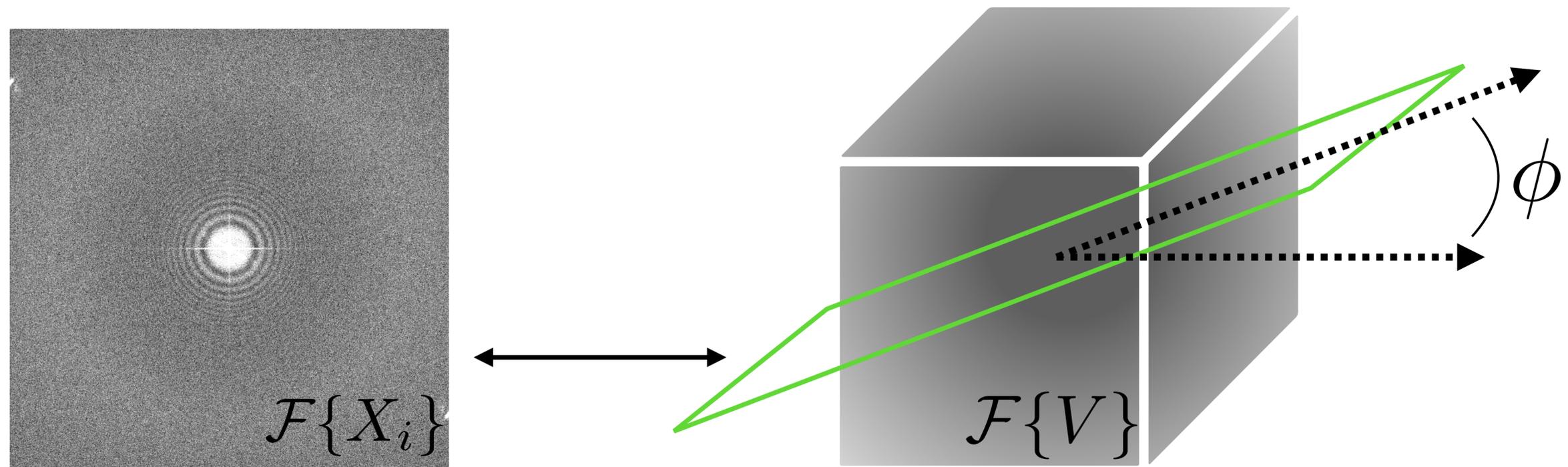


Fourier Space

Amplitude and phase as a function of frequency

Fourier Slice Theorem

- E-step: Extract Fourier slices out of the current Fourier volume and compute pose weights
- M-step: Insert Fourier transform of input image as slices of Fourier volume, according to pose weight



Fourier Slice Theorem: 2D FT is centrally oriented slice of 3D FT

Real space: $X_i = C_i * \mathcal{P}_{\phi_i} V + \eta_i$

Fourier space: $\mathcal{F}\{X_i\} = \mathcal{F}\{C_i\} \Theta_{\phi_i} \mathcal{F}\{V\}$

What are the tradeoffs in real vs Fourier space reconstruction?

Key Challenges in Optimization

1. Convergence to local optima due to poor volume initialization
2. Due to low SNR imaging, easily overfits to noise

Initialization of E-M Algorithm

- The E-M algorithm is guaranteed to improve the likelihood every iteration
- This suggests that given a random initialization of V , the algorithm will converge to a local optima
- To help find the global optimum, CryoSPARC (Punjani et al. 2017) introduced gradient descent on the objective to achieve a good starting volume

$$\hat{V}^{\text{MLE}} = \arg \max_V \ell(V) = \arg \max_V \sum_{i=1}^n \log \int_{\text{SO}(3) \times \mathbb{R}^2} \exp\left\{-\frac{\|X_i - C_i * \mathcal{P}_\phi V\|^2}{2\sigma^2}\right\} d\phi$$

$$V^{(t+1)} = V^{(t)} + \alpha_t \sum_{i \in B} \nabla_V \ell(V; X_i)$$

α_t Learning rate

B Batch of images

Preventing Overfitting to Noise

RELION (Scheres 2012) introduced a Bayesian framework for reconstruction:

$$\hat{V}^{\text{MAP}} = \arg \max_V \left[\underbrace{\log P(X_1, \dots, X_n | V)}_{\text{MLE Objective}} + \underbrace{\log P(V)}_{\text{Volume Prior (Regularization)}} \right]$$

A common prior is to assume each Fourier component is from a zero-mean Gaussian:

$$P(V) = \prod_{d=1}^{D^3} \frac{1}{2\pi\tau_d^2} \exp\left\{-\frac{|V_d|^2}{2\tau_d^2}\right\}$$

The frequency-dependent variance of the prior is sometimes optimized as well:

$$(\tau_d^2)^{(t)} = \frac{1}{2} |V_d^{(t)}|^2$$

Roadmap

- Overview of the cryo-EM pipeline
- Classical cryo-EM reconstruction
 - Homogeneous reconstruction
 - **Multiclass reconstruction**
- Modern heterogeneous reconstruction
 - CryoDRGN

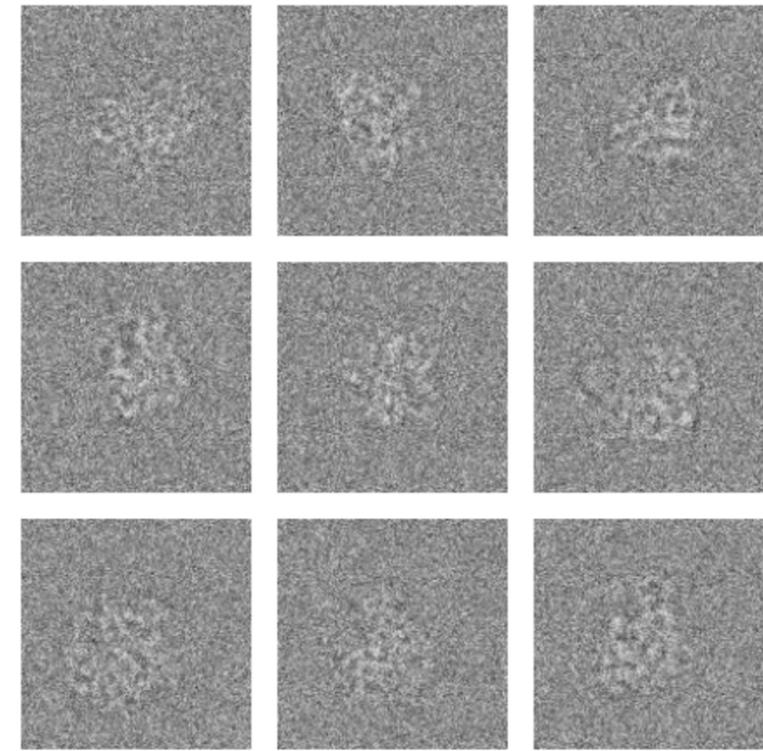
Multiclass Image Formation Model

Image Formation Model

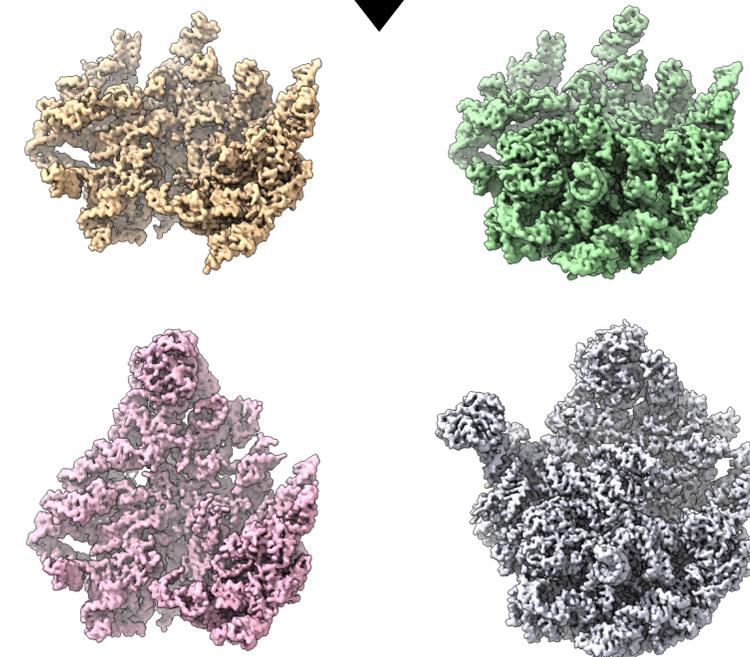
$$X_i = C_i * \mathcal{P}_{\phi_i} V_{a_i} + \eta_i$$

$$a_i \in \{1, \dots, K\}$$

Particle Class



[Jeon et al. 2024]



**Multiclass reconstruction problem:
Find optimal volumes $\{V_1, \dots, V_k\}$ given the data**

Multiclass Reconstruction

The MLE objective marginalizes over class assignments:

$$\hat{V}_1^{\text{MLE}}, \dots, \hat{V}_K^{\text{MLE}} = \arg \max_{V_1, \dots, V_K} \sum_{i=1}^n \log \sum_{k=1}^K P(X_i | \phi_i, V_k)$$

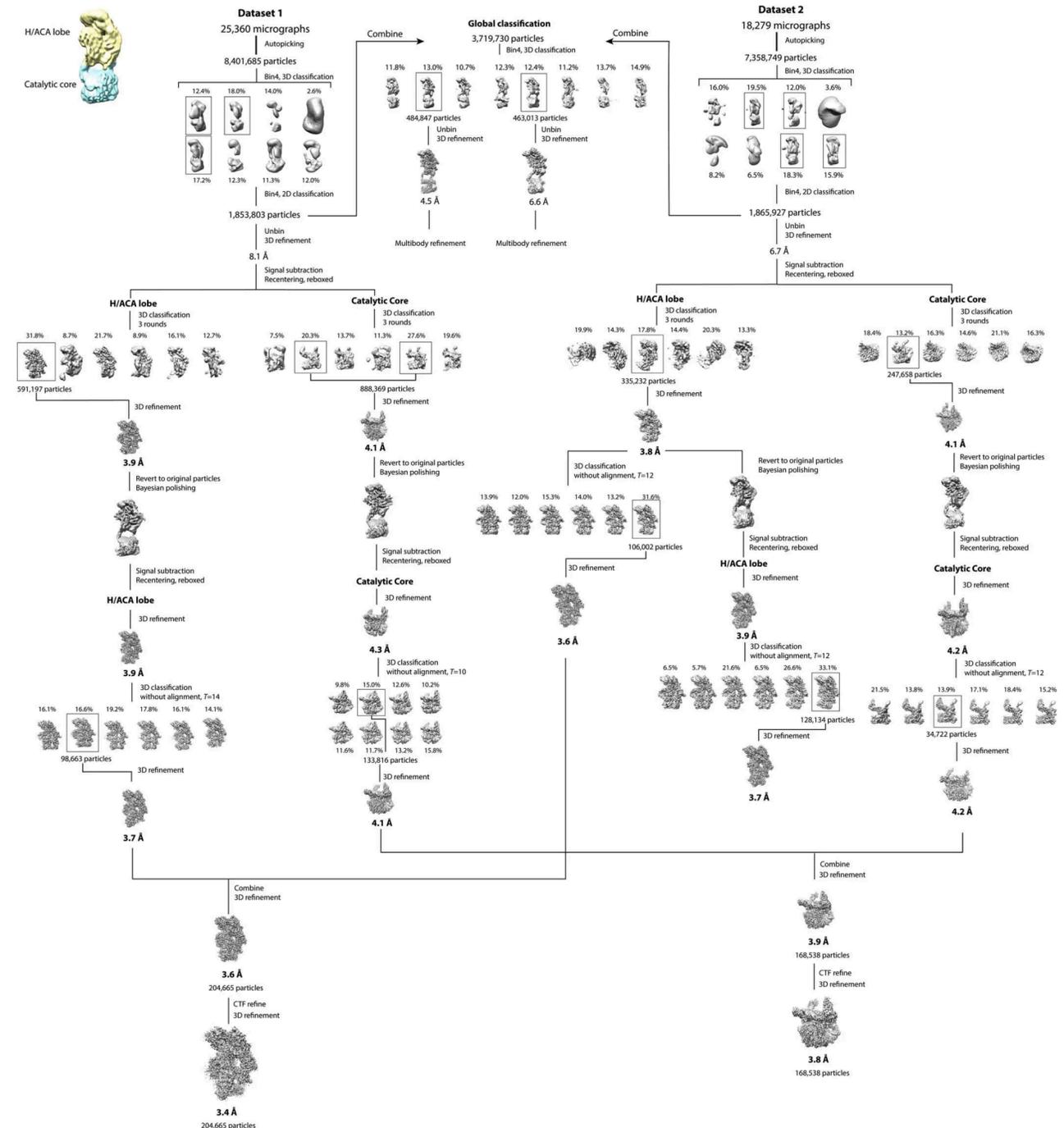
We can again use the E-M algorithm:

$$\mathbf{E}\text{-Step: } w_i(k) = P(a_i = k | V_1^{(t)}, \dots, V_K^{(t)}) = \frac{P(X_i | V_k^{(t)})}{\sum_{k' \in [K]} P(X_i | V_{k'}^{(t)})}$$

$$\mathbf{M}\text{-Step: } V_k^{(t+1)} = \arg \min_V \sum_{i=1}^n w_i(k) \|X_i - C_i * \mathcal{P}_{\phi_i} V\|^2$$

Practical Challenges in 3D Classification

- The discrete mixture model is not well-suited for continuous forms of heterogeneity
- Higher the number of classes K , the fewer the number of particles contributing to each volume
- Optimization especially sensitive to initial volumes
- *Ad hoc* processing pipelines involving iterative, hierarchical procedures with sweeps over K



Roadmap

- Overview of the cryo-EM pipeline
- Classical cryo-EM reconstruction
 - Homogeneous reconstruction
 - Multiclass reconstruction
- Modern heterogeneous reconstruction
 - **CryoDRGN**

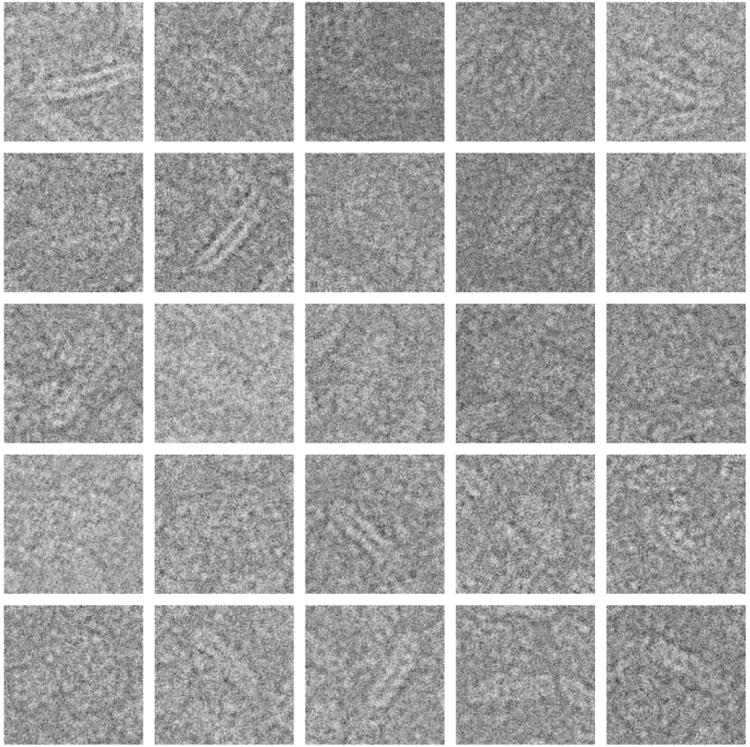
Heterogeneous Reconstruction

Image Formation Model

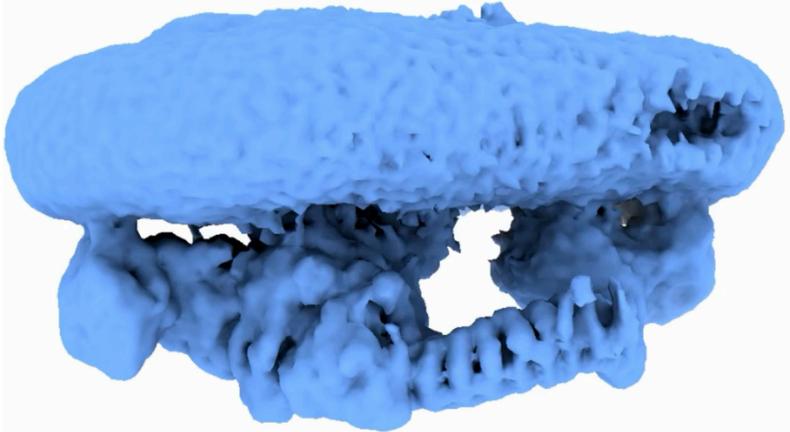
$$X_i = C_i * P_{\phi_i} \underbrace{V_{\theta}(z_i)} + \eta_i$$

Distribution of volumes

**Heterogeneous reconstruction problem:
Find optimal volume distribution V_{θ}
given the data**



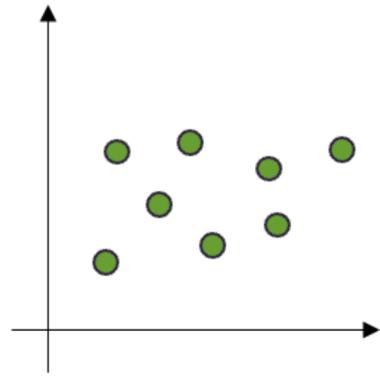
[EMPIAR-11043]



Latent Variable Models for Heterogeneous Reconstruction

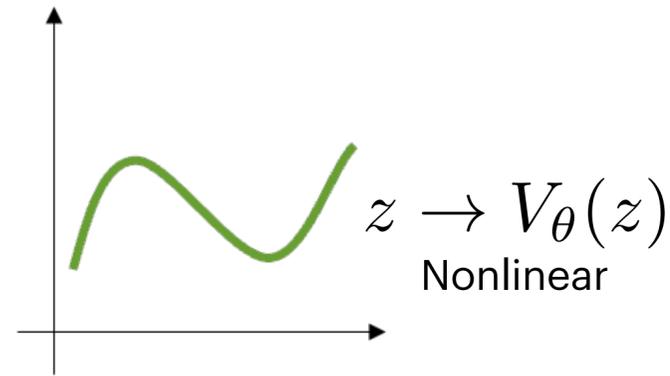
$$\{V_{\theta}(z), z \in Z\}$$

$$Z = \{1, \dots, K\}$$



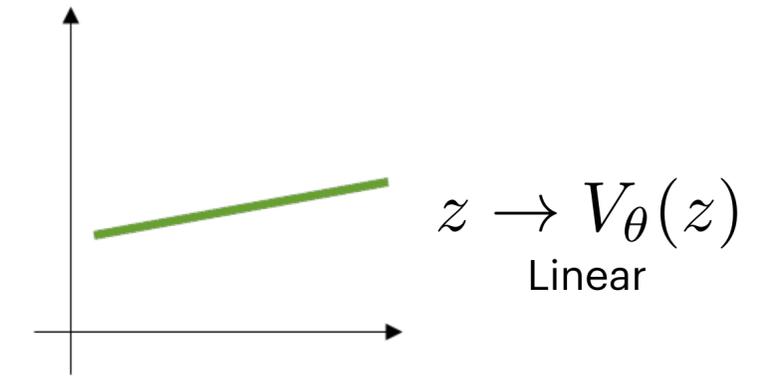
Discrete Set of Voxel Grids
RELION [1], CryoSPARC [2]

$$Z = \mathbb{R}^D$$



Non Linear Parameterizations [8, 9]

$$Z = \mathbb{R}^D$$

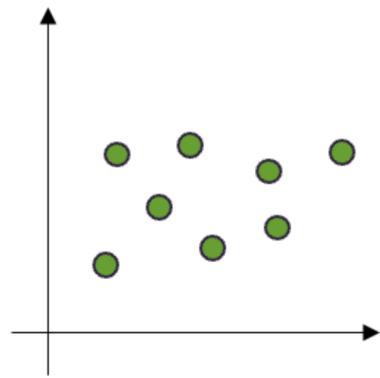


Linear Combination of Voxel Grids
3DVA, RECOVER,
Multibody

Latent Variable Models for Heterogeneous Reconstruction

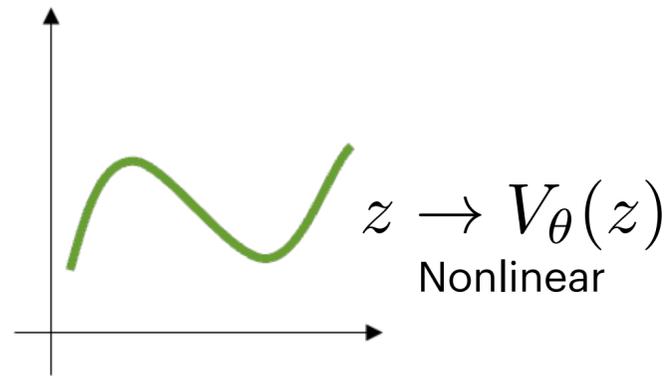
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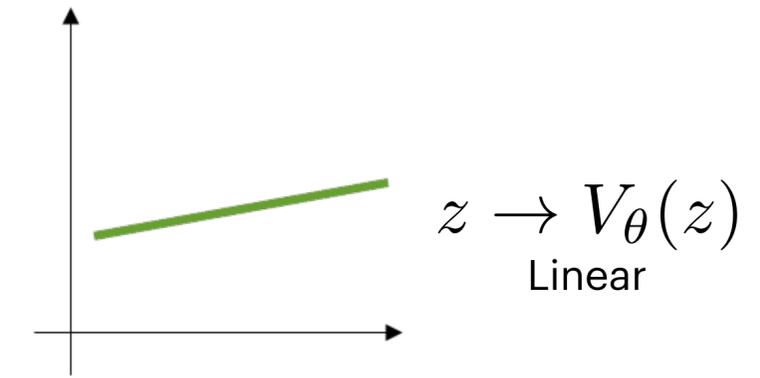
Discrete Set of Voxel Grids
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Linear Combination of Voxel Grids
3DVA, RECOVER,
Multibody

Neural Representations



CryoDRGN

(Zhong, Nat. Met., 2021)

Explicit: Multi-CryoGAN,
OPUS-DSD

Deformable GMMs



E2GMM

(Chen, Nat. Met., 2021)

HEMNMA, CryoSTAR
Dynamight, Cryofold, ...

Flow Field

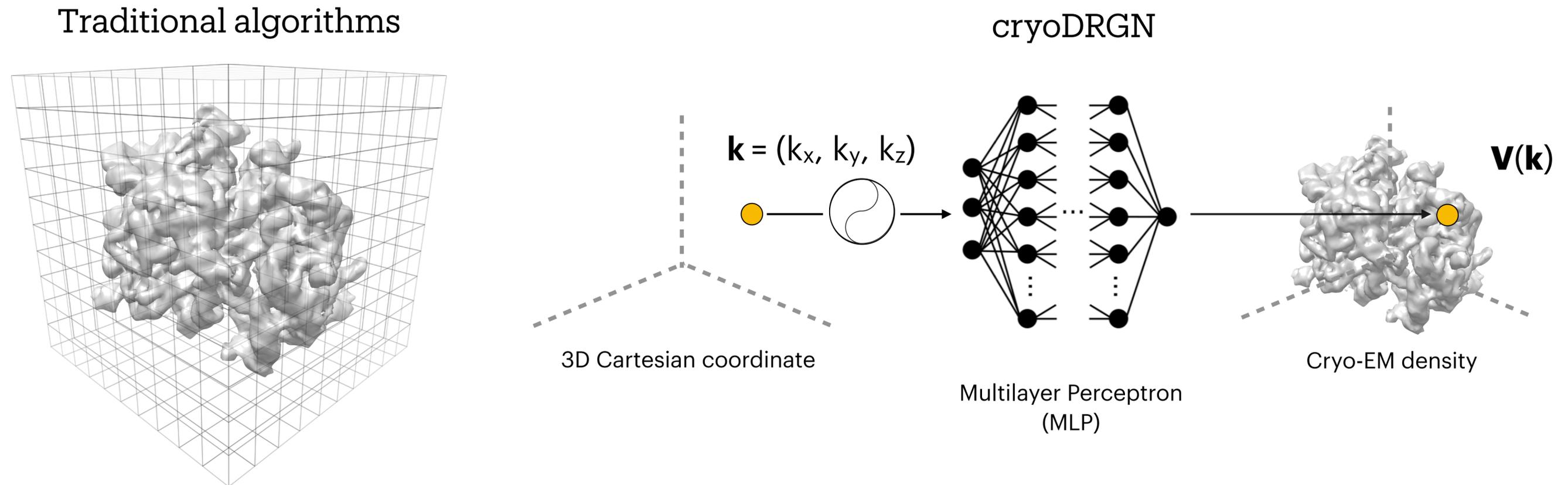


3DFLEX

(Punjani, Nat. Met., 2023)

Coordinate-based neural networks for 3D volumes

Key idea: Instead of representing the structure as discrete points on a 3D lattice, learn a *continuous* function, $V : \mathbb{R}^3 \rightarrow \mathbb{R}$

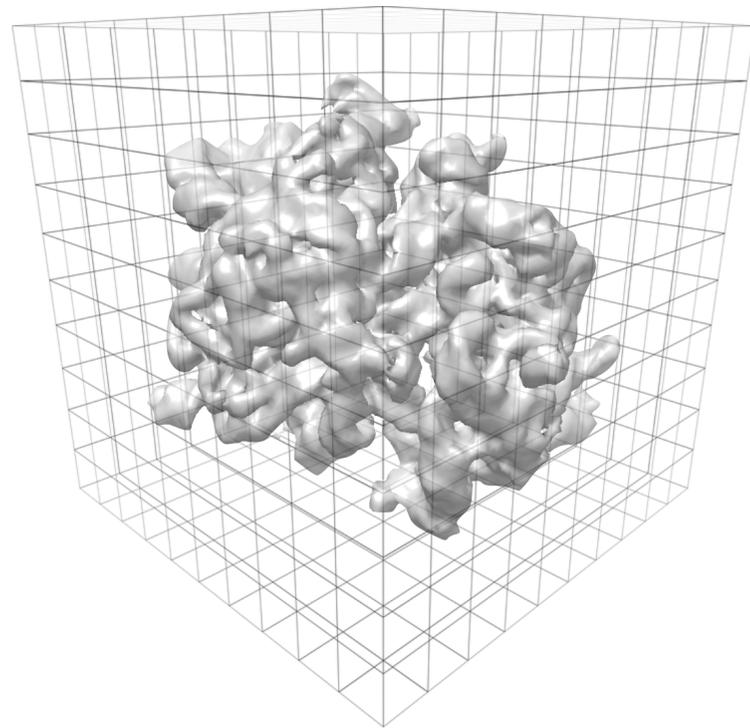


CryoDRGN structures are parameterized as a **neural field** instead of a voxel array

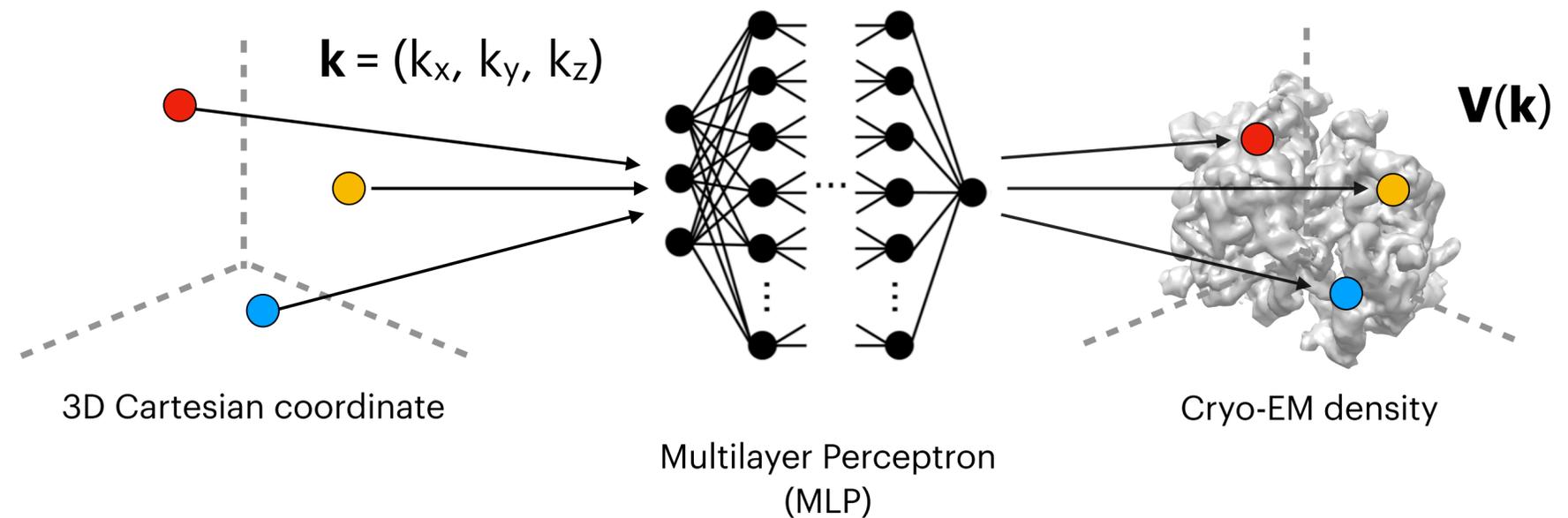
Coordinate-based neural networks for 3D volumes

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Traditional algorithms



cryoDRGN

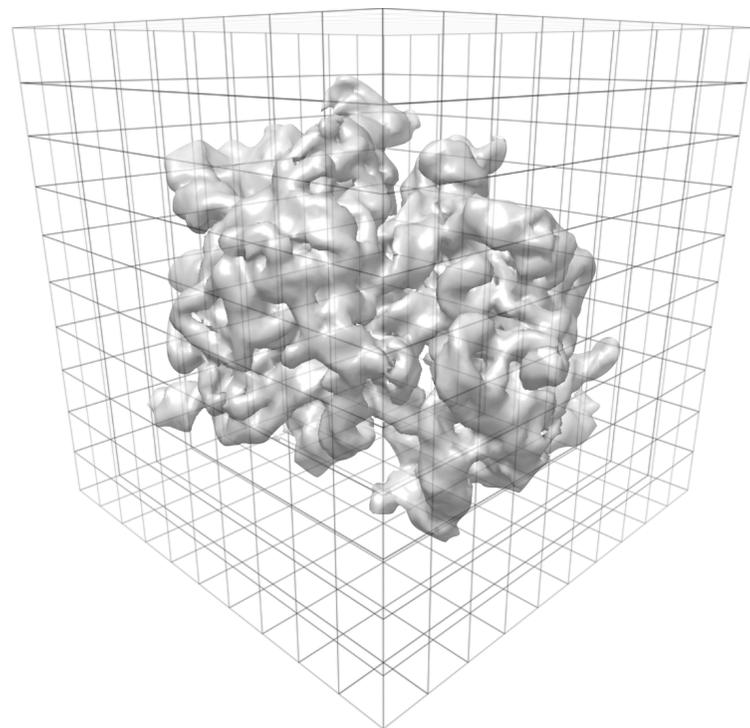


To construct a volume, evaluate the function at different spatial frequencies

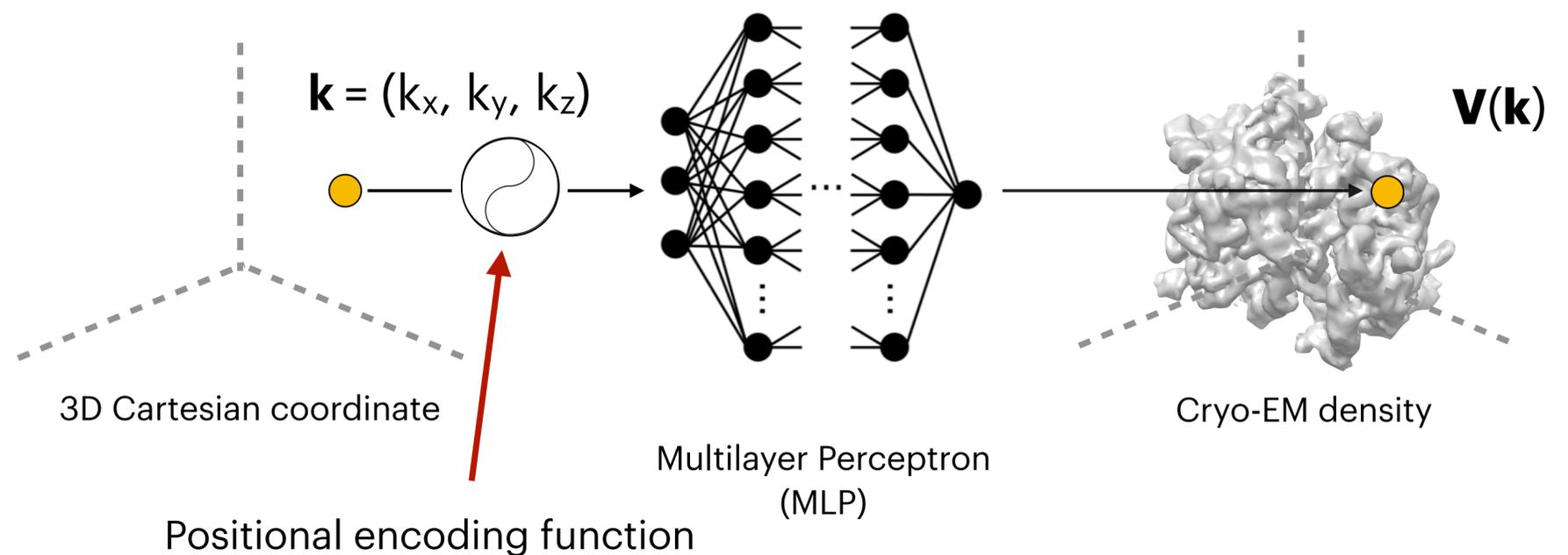
Coordinate-based neural networks for 3D volumes

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cryoDRGN

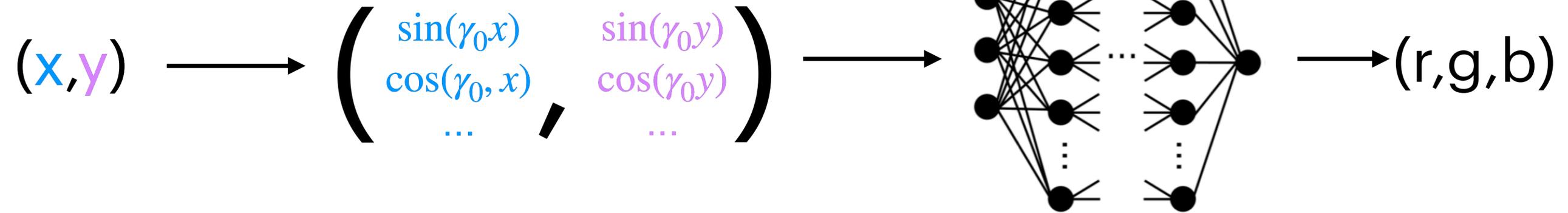


$$pe^{(2i)}(k_j) = \sin(k_j D \pi (2/D)^{2i/D}), \quad i = 1, \dots, D/2; k_j \in k$$

$$pe^{(2i+1)}(k_j) = \cos(k_j D \pi (2/D)^{2i/D}), \quad i = 1, \dots, D/2; k_j \in k$$

Sinusoidal featurization of inputs

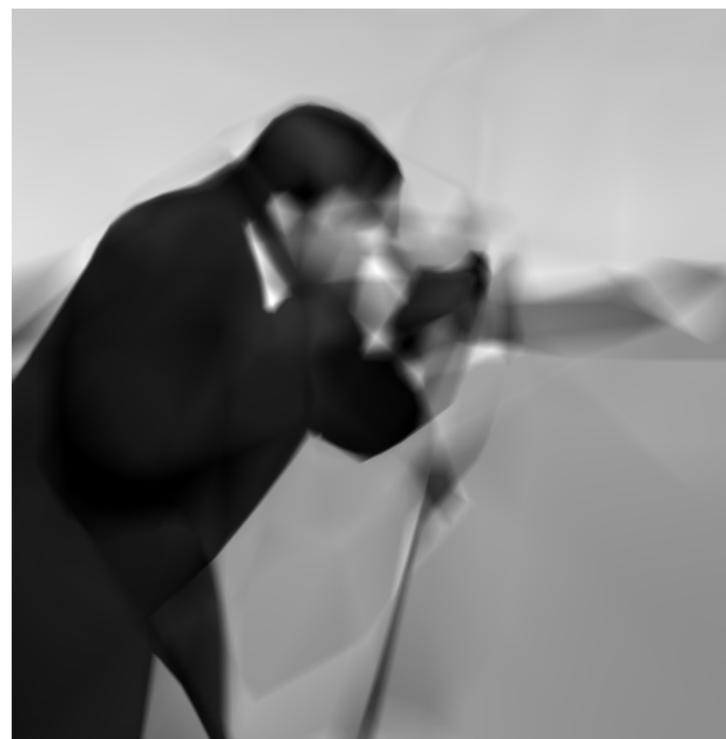
A toy example: Use an MLP to learn an image



Ground truth



No sinusoidal encoding



With sinusoidal encoding

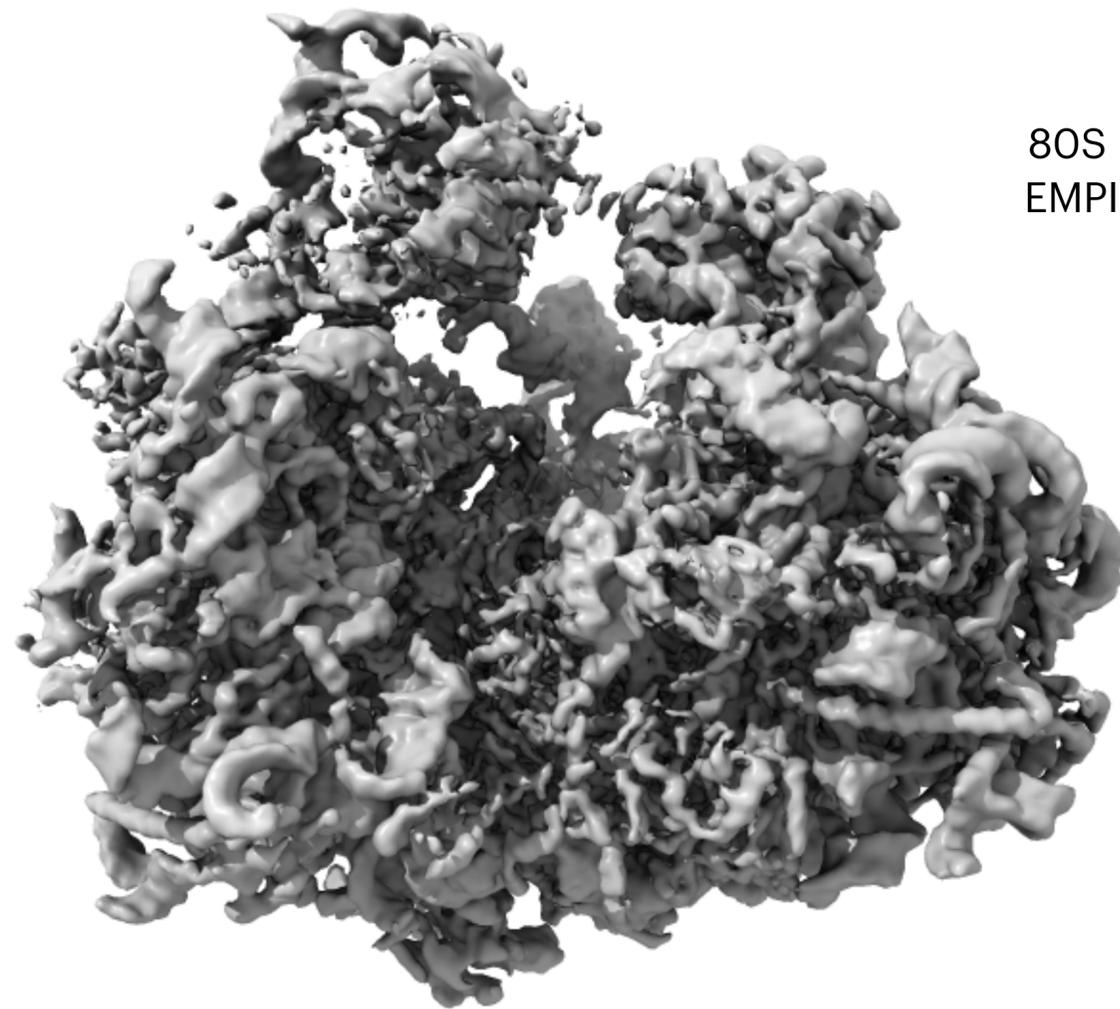


Neural fields can learn high resolution maps

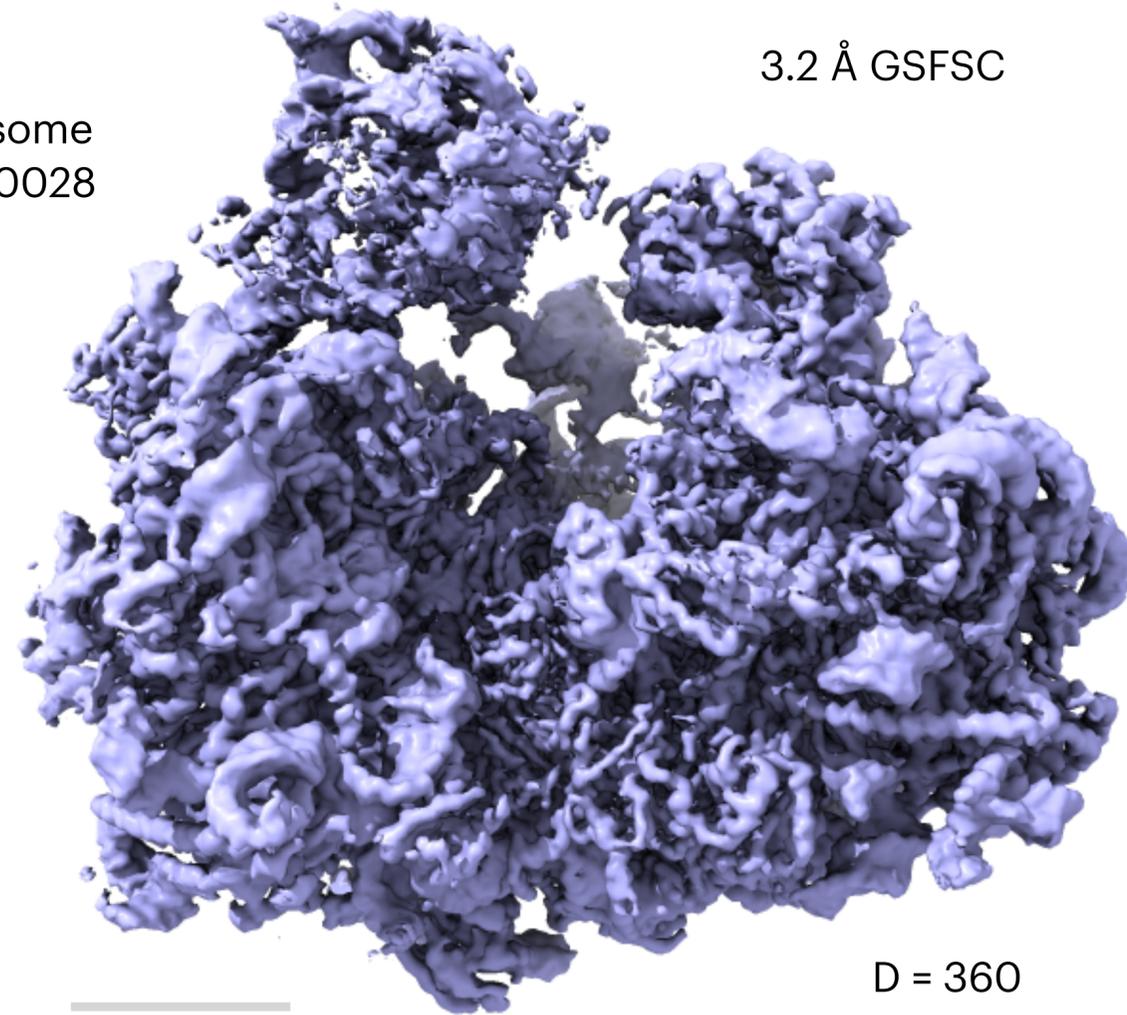
Train the cryoDRGN decoder (with no latent variable input) on images from EMPIAR-10028

Neural network representation

Voxel-based representation



80S ribosome
EMPIAR 10028



3.2 Å GSFSC

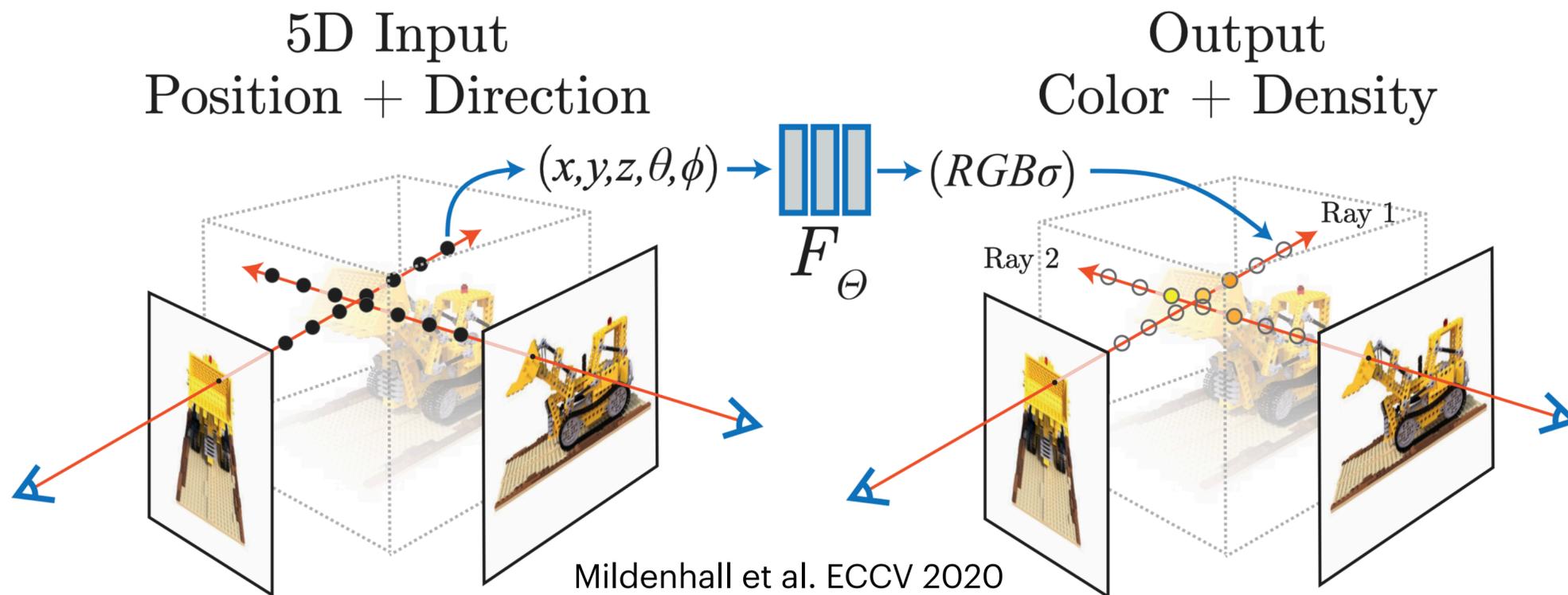
D = 360

50 Å

1024x10 architecture
50 epochs

Neural fields show broad applicability

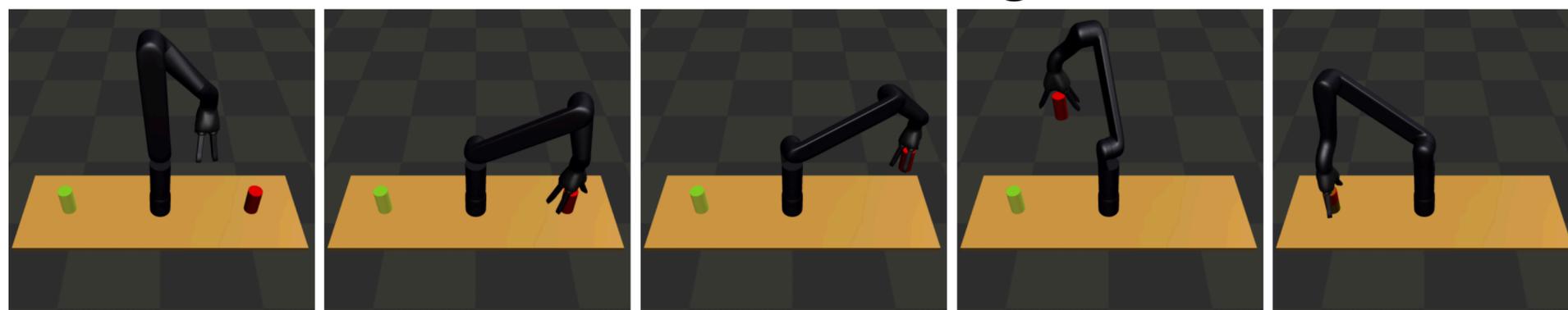
Neural Radiance Fields



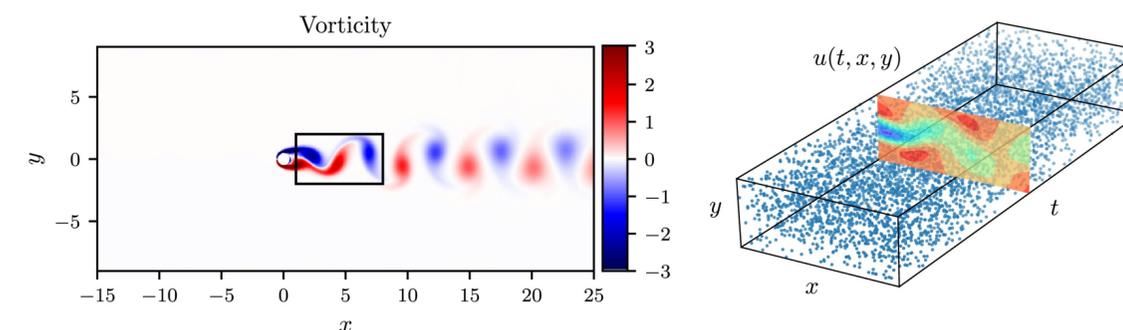
Scene Representation



Robotic Planning



Physics



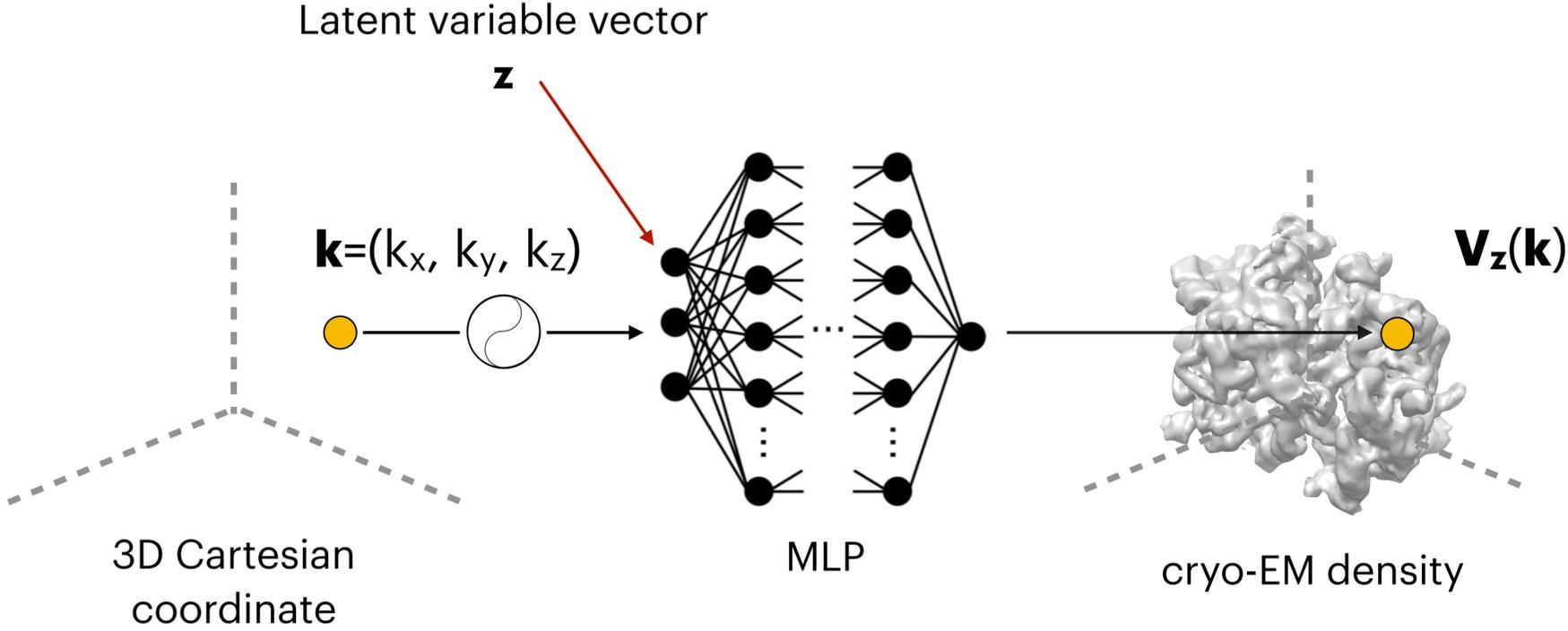
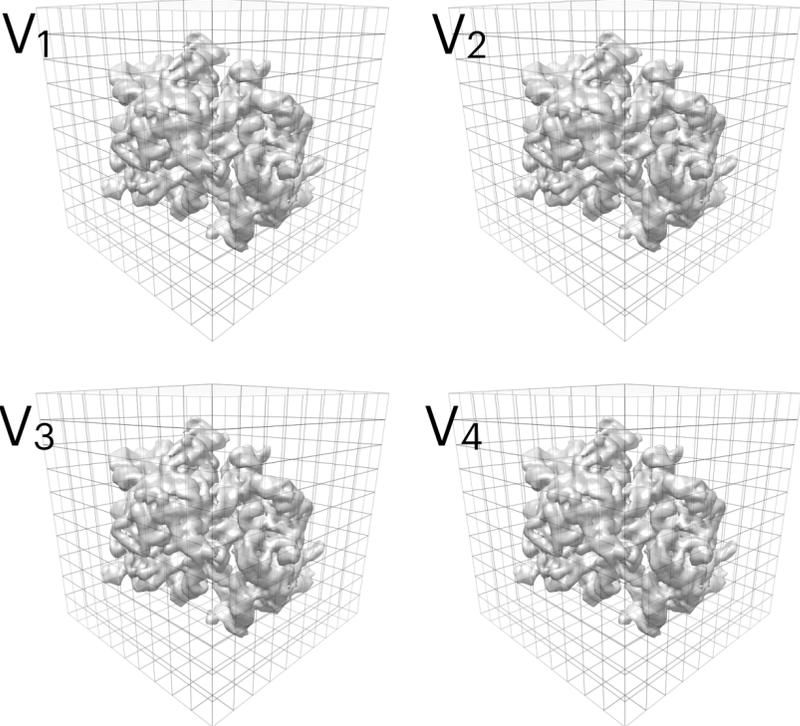
Latent variable models for heterogeneous structures

Multiclass reconstruction

V_z , where $z \in \{1, \dots, K\}$

cryoDRGN 

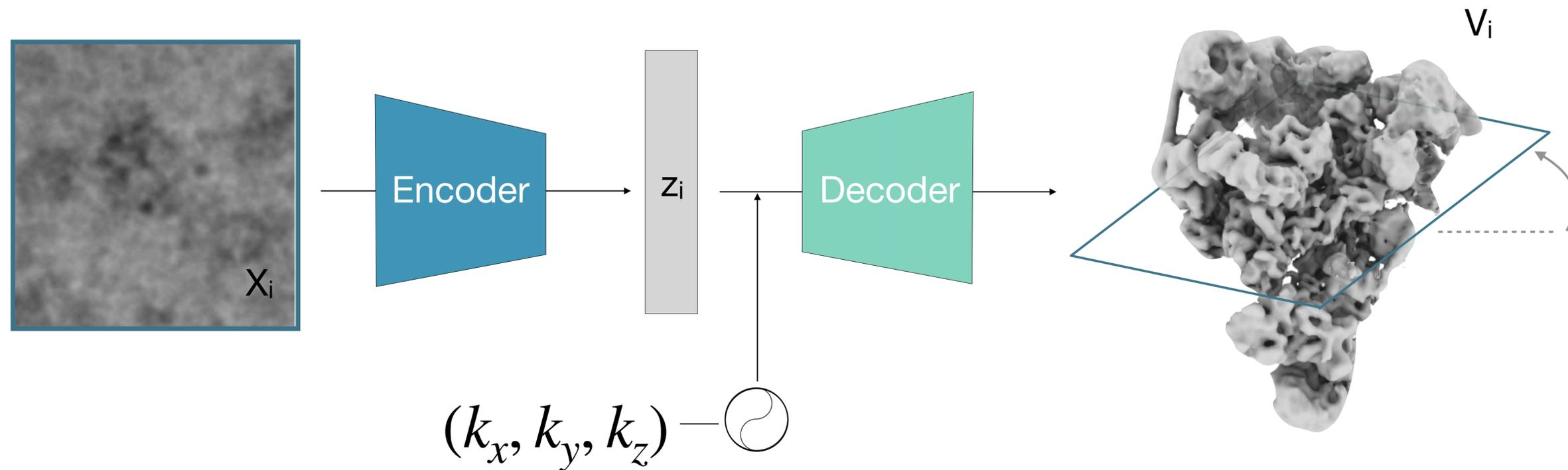
$$z \rightarrow V_\theta(z), z \in \mathbb{R}^D$$



CryoDRGN Architecture

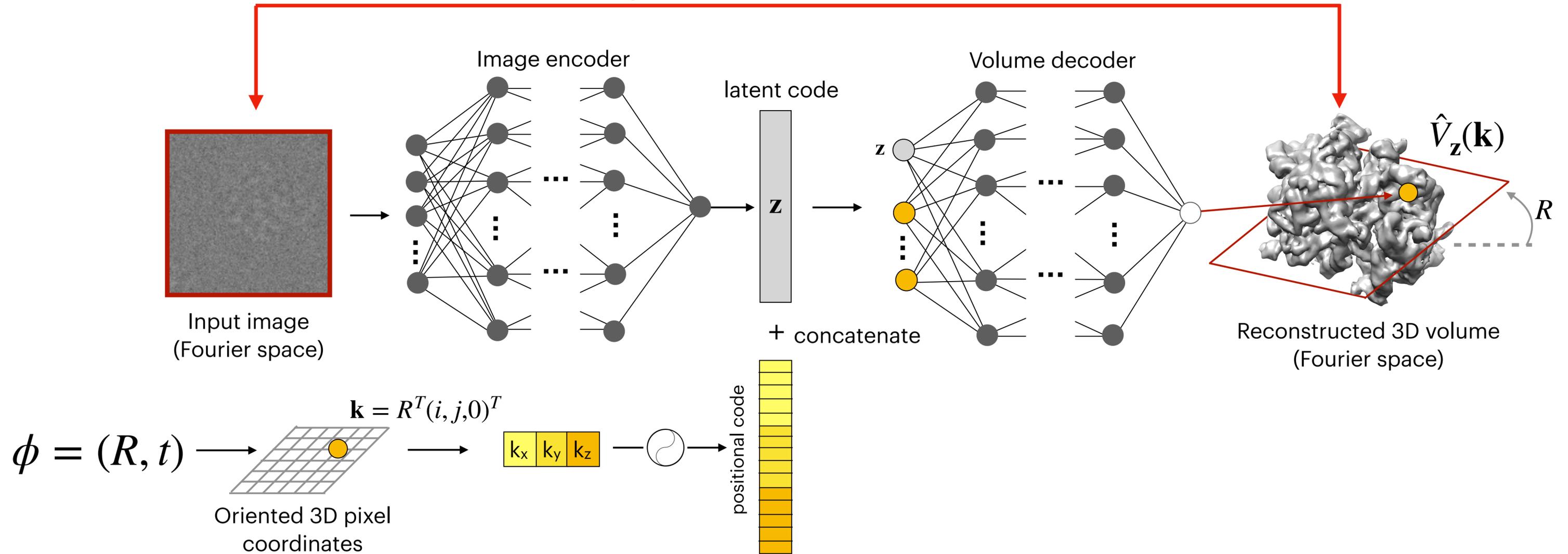
Variational autoencoder

- Given a particle, the **encoder** predicts a latent variable z describing the particle's conformation
- Given z and spatial frequencies, the **decoder** outputs cryo-EM densities



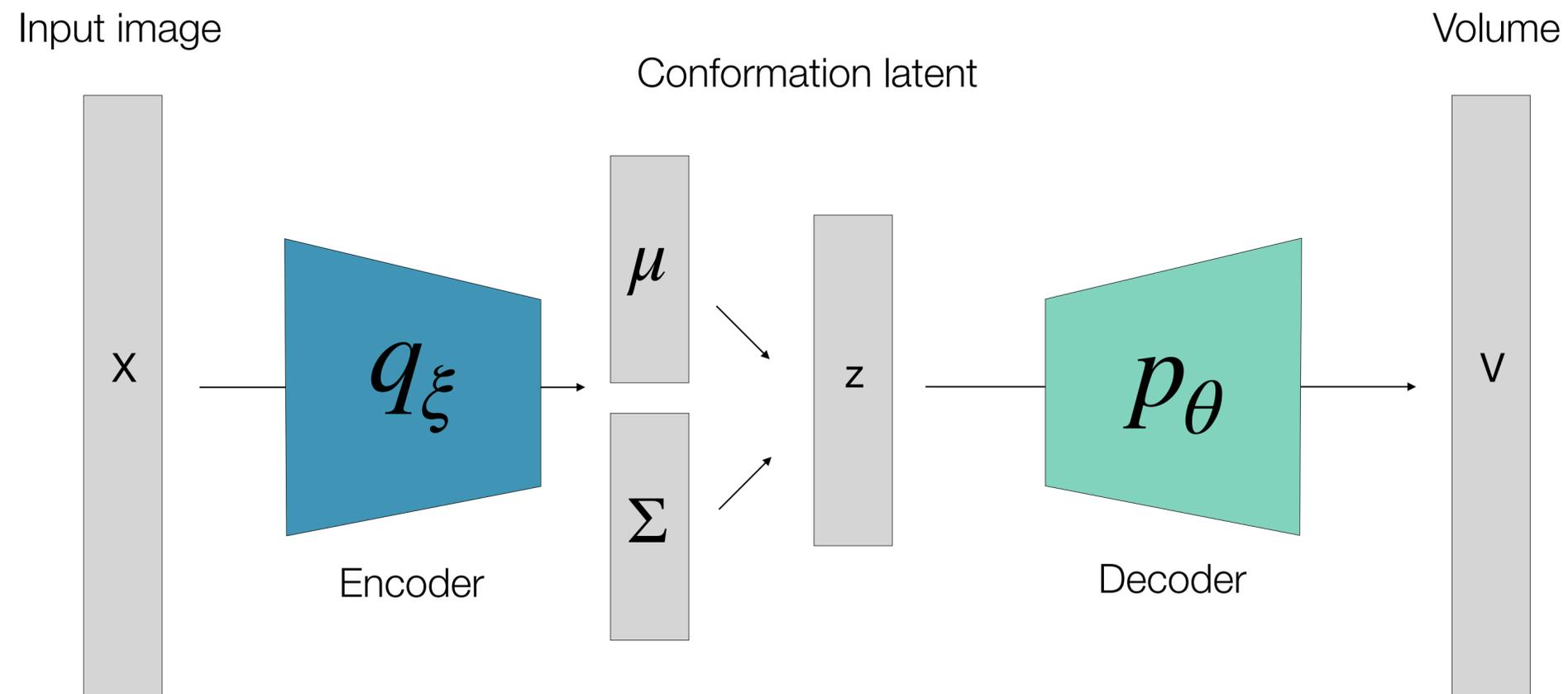
CryoDRGN Training

Image Reconstruction Error



- Input images are oriented central slices of the reconstructed volume by the Fourier slice theorem
- Training loss is mean squared error between input image and reconstructed image (plus a KL-divergence term)

Amortized Latent Inference



The VAE extends the AE as inference of a probabilistic model — “a regularized autoencoder”

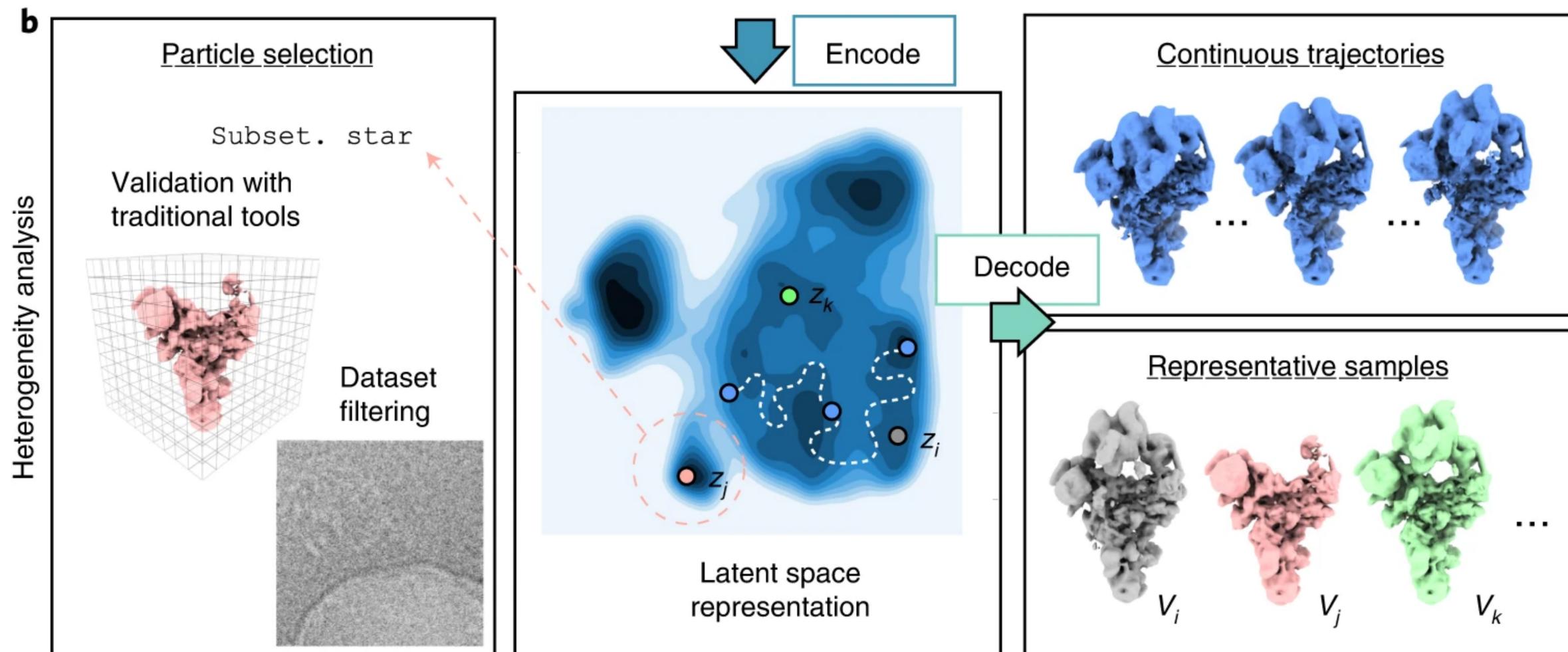
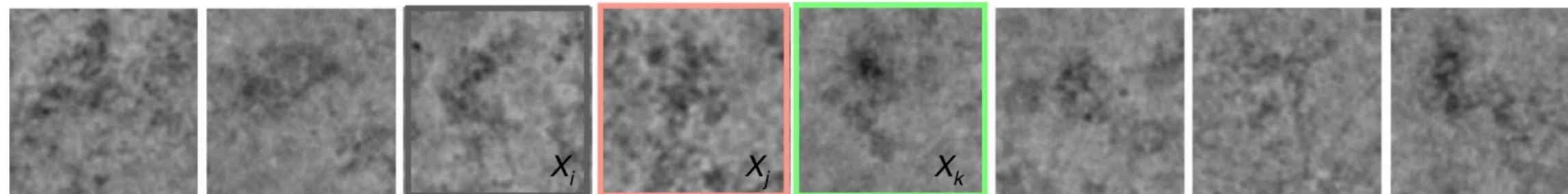
$$\mathcal{L}_{VAE}(X; \theta, \xi) = \underbrace{\mathbb{E}_{q_\xi(z|X)}[\log p_\theta(X|z)]}_{\text{Reconstruction error}} - \underbrace{KL(q_\xi(z|X) || p(z))}_{\text{Regularization}}$$

Reconstruction error

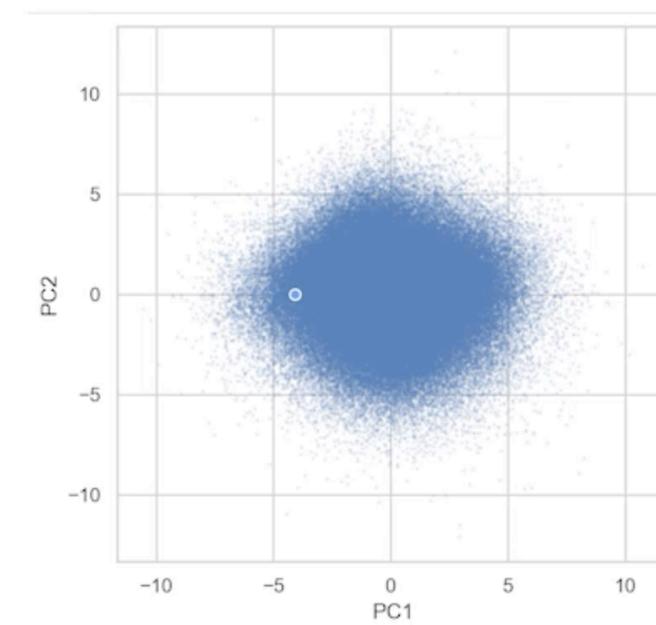
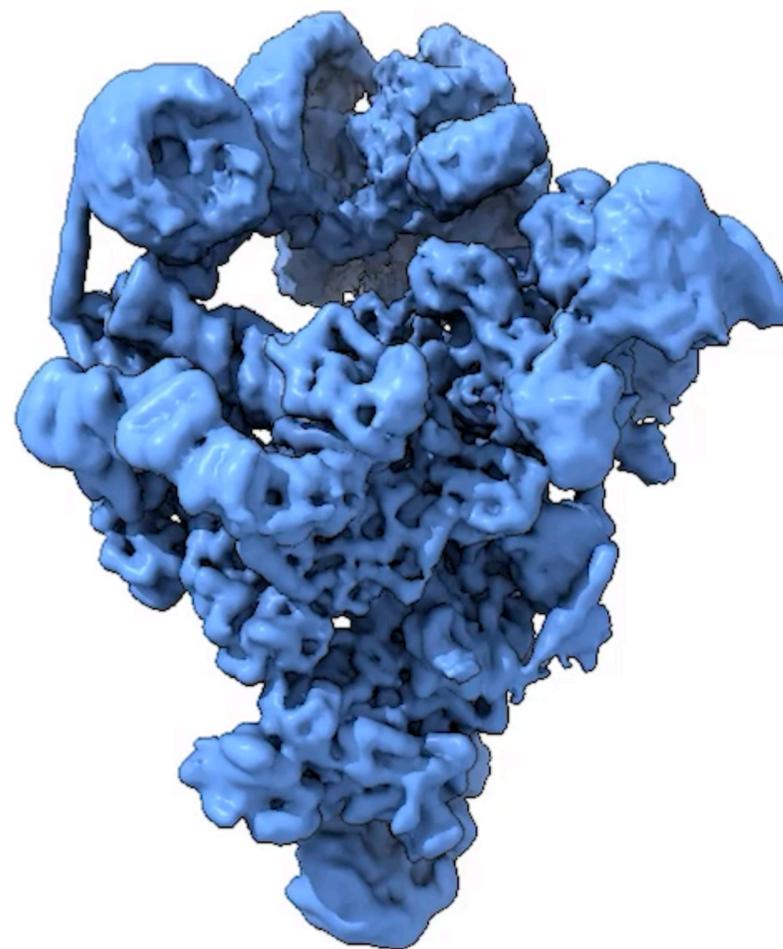
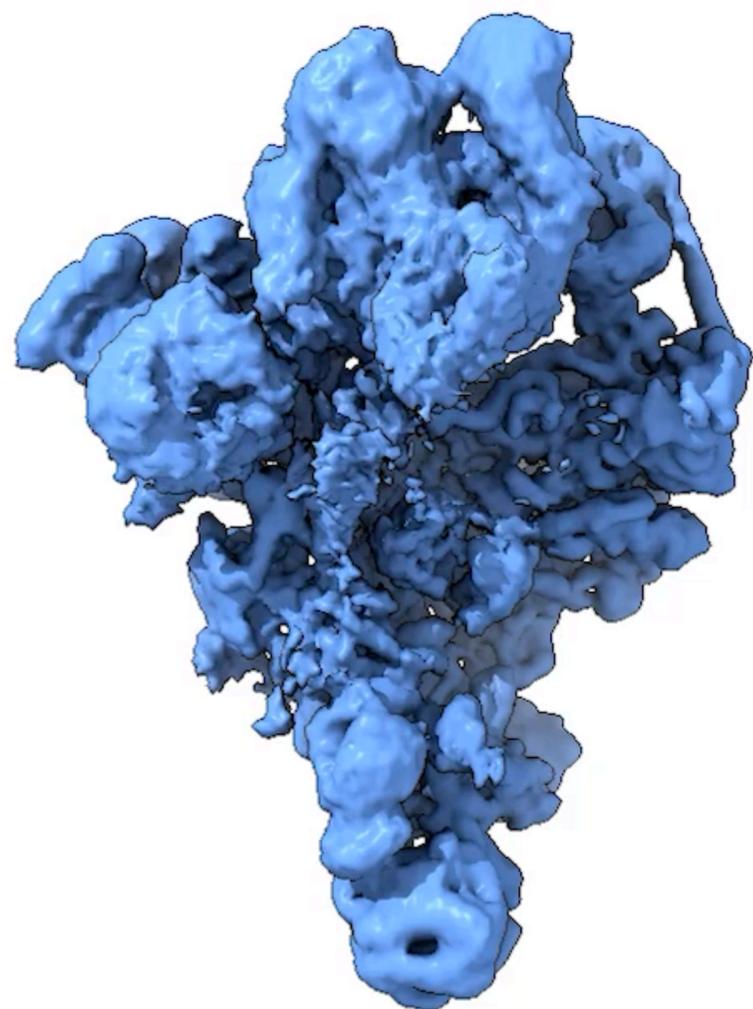
Regularization

CryoDRGN Inference

- Use the encoder network to evaluate the latent embedding \mathbf{z} for each image
- Use the decoder network to generate \mathbf{V} at different values of \mathbf{z}



Reconstructing continuous variability of the spliceosome

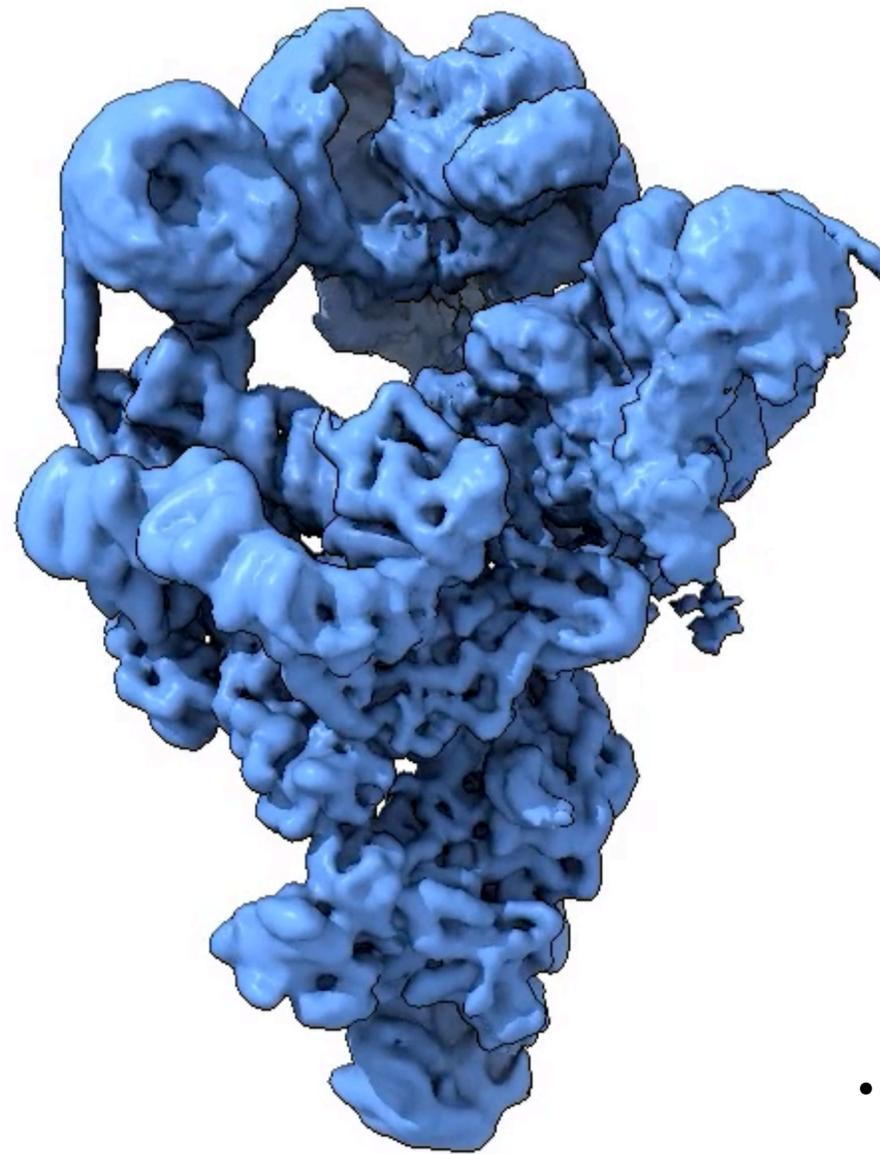
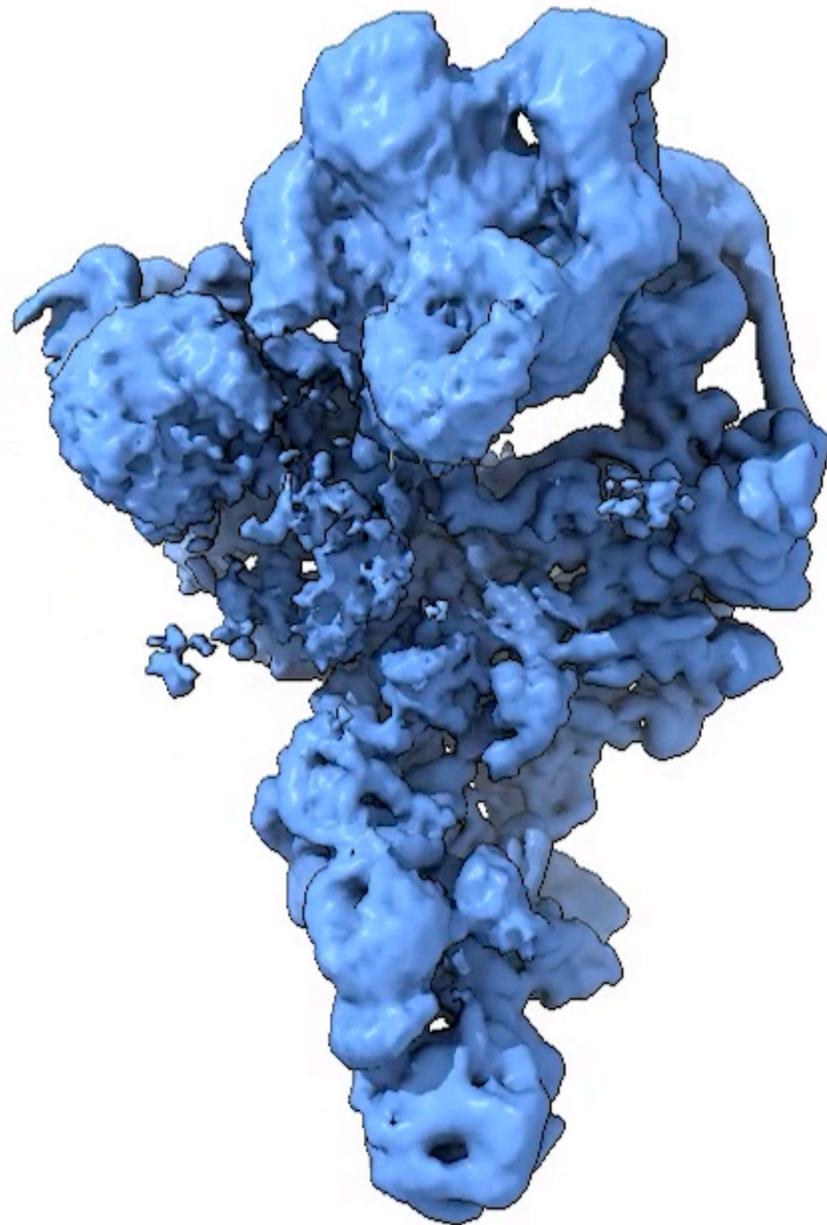


[EMPIAR-10180]

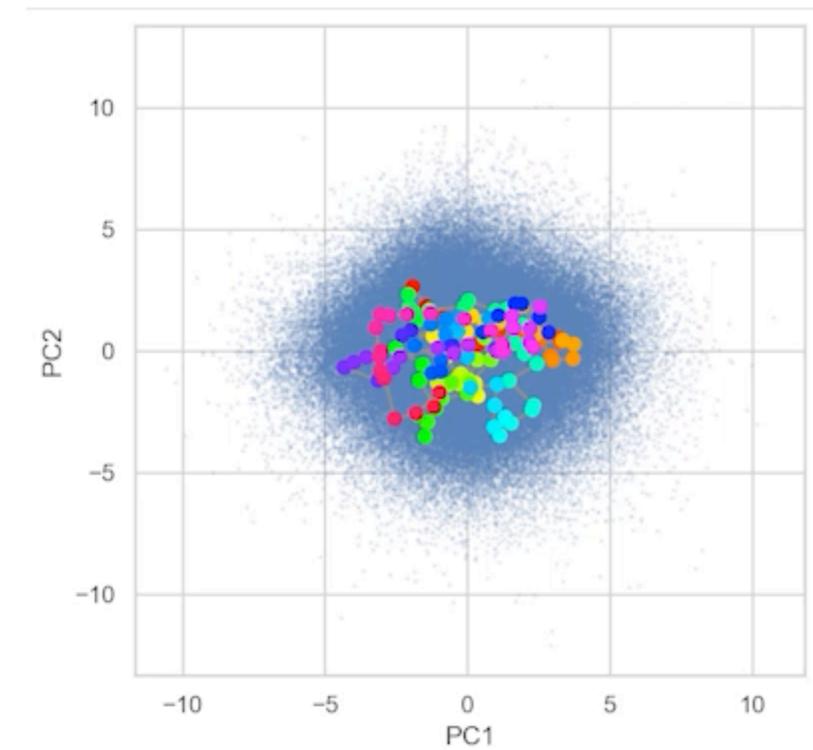
`cryodrgn pc_traversal`

Trajectories along principle component axis of the latent space show variability within dataset

Generating trajectories with a graph traversal algorithm



`cryodrgn graph_traversal`



[EMPIAR-10180]

- Explore the learned distribution
- Extended with latent space diffusion models (Kreis, Dockhorn, Li, Zhong 2022)

Summary

- Cryo-EM captures proteins in their “near-native” state, sampled from an “equilibrium” distribution of conformations
- Principled probabilistic techniques underlie cryo-EM reconstruction
- Tools for heterogeneous reconstruction encode different assumptions about the heterogeneity present in the data
- CryoDRGN’s implicit neural representation provides a expressive model of heterogeneity

